



ALMA MATER STUDIORUM  
UNIVERSITÀ DI BOLOGNA

ARCHIVIO ISTITUZIONALE  
DELLA RICERCA

Alma Mater Studiorum Università di Bologna  
Archivio istituzionale della ricerca

Standardization of hemipelvis alignment for in vitro biomechanical testing

This is the final peer-reviewed author's accepted manuscript (postprint) of the following publication:

*Published Version:*

Standardization of hemipelvis alignment for in vitro biomechanical testing / Morosato F.; Traina F.; Cristofolini L.. - In: JOURNAL OF ORTHOPAEDIC RESEARCH. - ISSN 0736-0266. - STAMPA. - 36:6(2018), pp. 1645-1652. [10.1002/jor.23825]

*Availability:*

This version is available at: <https://hdl.handle.net/11585/722710> since: 2021-03-07

*Published:*

DOI: <http://doi.org/10.1002/jor.23825>

*Terms of use:*

Some rights reserved. The terms and conditions for the reuse of this version of the manuscript are specified in the publishing policy. For all terms of use and more information see the publisher's website.

This item was downloaded from IRIS Università di Bologna (<https://cris.unibo.it/>).  
When citing, please refer to the published version.

(Article begins on next page)



This is the final peer-reviewed accepted manuscript of:

**Standardization of hemipelvis alignment for in vitro biomechanical testing**

Federico Morosato, Francesco Traina, Luca Cristofolini

J Orthop Res. 2018 Jun;36(6):1645-1652. Epub 2017 Dec 19

The final published version is available online at:

<https://doi.org/10.1002/jor.23825>

Rights / License:

The terms and conditions for the reuse of this version of the manuscript are specified in the publishing policy. For all terms of use and more information see the publisher's website.

# Standardization of hemipelvis alignment for *in vitro* biomechanical testing

Federico Morosato, MEng<sup>1</sup>, Francesco Traina, MD<sup>2</sup>, Luca Cristofolini, Ph.D. <sup>1</sup>

<sup>1</sup> Department of Industrial Engineering, School of Engineering and Architecture, Alma Mater Studiorum - Università di Bologna, Bologna, Italy

<sup>2</sup> Second Clinic of Orthopaedics and Traumatology, Rizzoli Orthopaedic Institute, Bologna, Italy

## ***Submitted to: J. Orthopaedic Research***

***Version.0:*** 28<sup>th</sup> June 2017

***Version.1:*** 5<sup>th</sup> October 2017

## ***Statistics:***

Word count (manuscript):	3514
Word count (abstract):	248
Figures:	7
Tables:	1
References:	45

## ***Corresponding author:***

Luca Cristofolini  
Department of Industrial Engineering  
School of Engineering and Architecture  
University of Bologna  
Via Umberto Terracini 24/26  
40131 Bologna, Italy  
Phone: +39 051 2090148  
e-mail: [luca.cristofolini@unibo.it](mailto:luca.cristofolini@unibo.it)

***Author Contributions Statement:*** (1) all the three authors gave a substantial contribution to research design, the acquisition, the analysis and the interpretation of data; (2) all the three authors gave a substantial contribution to drafting and critically revising the paper; (3) all authors have read and approved the final submitted manuscript.

***Running title:*** Hemipelvis alignment for biomechanical tests

1 **ABSTRACT**

2 Although *in vitro* biomechanical tests are regularly performed, the definition of a suitable  
3 reference frame for hemipelvic specimens is still a challenge. The aims of the present  
4 study were to: (1) define a reference frame for the human hemipelvis suitable for *in vitro*  
5 applications, based on robust anatomical landmarks; (2) identify the alignment of a  
6 hemipelvis based on the alignment of a whole pelvis (including right/left and male/female  
7 differences); (3) identify the relative alignment of the proposed *in vitro* reference frame  
8 with respect to a reference frame commonly used in gait analysis; (4) create an *in vitro*  
9 alignment procedure easy, robust and inexpensive; (5) quantify the intra-operator  
10 repeatability and inter-operator reproducibility of the procedure. A procedure to  
11 univocally identify the anatomical landmarks was created, exploiting the *in vitro*  
12 accessibility of the specimen's surface. Through the analysis on 53 CT scans (106  
13 hemipelvises), the alignment of the hemipelvis based on the alignment of a whole pelvis  
14 was analyzed: differences between male/female and right/left hemipelvises were not  
15 statistically significant. To overcome the uncertainty in the identification of the acetabular  
16 rim, a standard acetabular plane was defined. An alignment procedure was developed to  
17 implement such anatomical reference frame. The intra-operator repeatability and the  
18 inter-operator reproducibility were quantified with four operators, on male and female  
19 hemipelvises. The intra-operator repeatability was better than 1.5°. The inter-operator  
20 reproducibility was better than 2.0°. Alignment in the transverse plane was the most  
21 repeatable. The presented procedure to align hemipelvic specimens is sufficiently robust,  
22 standardized, and accessible.

23 **Keywords:** Anatomical reference frame; *in vitro* alignment; biomechanical testing;  
24 hemipelvis; acetabular plane

25

## 26 1. INTRODUCTION

27 Reference frames and landmarks are of paramount importance in biomechanics <sup>1; 2</sup>, to  
28 allow comparisons between different clinical, numerical or *in vitro* studies.

29 Standardisation of the reference frame is extremely important for *in vitro* biomechanical  
30 tests <sup>2-6</sup>. It enables the correct alignment of the specimen and applied loads, in order to  
31 reproduce a physiological loading condition. With the definition of reproducible testing  
32 conditions, it is possible to compare different datasets of different studies.

33 Reference frames and landmarks for the pelvic bone are adopted in different applications  
34 <sup>1; 2; 7-14</sup>. Reference frames used for the analysis of medical images are qualitative in most  
35 cases <sup>7-9</sup>. In example, to evaluate the pelvic tilt and sacral slope surgeons generally use  
36 lateral radiographs, in combination with anatomical landmarks, assuming that the x-ray  
37 frame is aligned with the anatomical planes. However, identification of these landmarks  
38 depends on multiple factors like image quality and the position assumed by the patient.  
39 For this reason, information that can be extracted from medical images is extremely  
40 operator-dependent. *In vivo* applications (i.e. gait analysis) deal with reference frames  
41 defined by palpable anatomical landmarks <sup>1; 10; 11</sup>. Landmarks routinely used in clinical  
42 practice are the most accessible ones, while those that would cause patient discomfort are  
43 avoided (e.g. pubic tubercle). Identification of the landmarks is heavily affected by the  
44 presence of soft tissue. These considerations dictate some constraint to the reference  
45 frames that can be adopted for *in vivo* applications. Surgical navigation adopts reference  
46 frames both for the pre-operative planning and for intra-operative deployment <sup>12-14</sup>.  
47 Similarly, *in silico* applications rely on mathematical models derived from CT scans. Due  
48 to the possibility to “navigate” the bone, identification of anatomical landmarks on CT

49 scans (which contain more detailed information) is more accurate. All the published  
50 reference frames for the human pelvis<sup>4; 15; 16</sup> rely on palpable landmarks that can be  
51 reached non-invasively:

- 52 • Anterior Superior Iliac Spine (ASIS) defined as the most prominent point on the  
53 iliac surface;
- 54 • Posterior Superior Iliac Spine (PSIS) defined as the upper and most posterior point  
55 of the iliac crest;
- 56 • Pubic Tubercle (PT) defined as a prominent forward-projecting tubercle on the  
57 upper border of the medial portion of the superior ramus of the pubis.

58 The Anterior Pelvic Plane (APP) is most widely used clinically<sup>17-19</sup>. It is defined by the  
59 ASISs and the PTs. Despite the physiological range of tilt of the APP, it is assumed to be  
60 roughly vertical in the standing position (anatomical neutral position, ANP)<sup>20; 21</sup>.

61 A dedicated reference frame for *in vitro* biomechanical testing can rely on anatomical  
62 landmarks that are accessed directly on the specimen (after the removal of soft tissues).  
63 For this reason, *in vitro* reference frames are more robust and less operator-dependent than  
64 *in vivo* ones, in which landmarks need to be identified non-invasively.

65 Despite the considerations above, only a few studies can be found where a suitable  
66 reference frame is defined for the pelvis and hemipelvis<sup>22; 23</sup>. It is very important to  
67 underline that hemipelvic specimens are frequently adopted for *in vitro* purposes<sup>24-26</sup>. All  
68 the reference frames described above rely on landmarks over the whole pelvis, and cannot  
69 be implemented on a hemipelvis alone. Currently, there is no consensus on a specific  
70 procedure for aligning a hemipelvis. Hence, in order to define a reference frame for the

71 hemipelvis, it is necessary to determine its alignment with respect to the whole pelvis.  
72 The few previous studies dealing with hemipelvic specimens lack detail about its  
73 alignment: Lewton *et al.* (2015) specified the direction of loads, defined as angles  
74 measured relative to the long axis of the pelvis but no reference frame was defined <sup>23</sup>.  
75 Preece *et al.* (2008) proposed a practical method based on the ANP; however more  
76 information about the alignment procedure were not stated <sup>27</sup>.

77 The acetabular plane, which is defined as the plane tangent to the acetabular rim is often  
78 used clinically <sup>28; 29</sup>. The alignment of the acetabular plane was investigated by Murray <sup>30</sup>.  
79 In his work, he identified three definitions for acetabular inclination and anteversion:  
80 radiological, operative and anatomical. Surgeons usually adopt the orientation of  
81 acetabular plane as guide for surgical navigation, since it is easily identified through  
82 clinical imaging <sup>28; 29</sup>. The acetabular plane was also adopted in different *in vitro* tests <sup>24-</sup>  
83 <sup>26; 31</sup>. However, the irregular shape of the acetabular rim makes the identification of this  
84 plane subjective <sup>32; 33</sup>.

85 Recently van Arkel *et al.* (2016) described an *in vitro* method to align a hemipelvic  
86 specimen, based on the reference frame recommended by the International Society of  
87 Biomechanics (ISB) <sup>4; 22</sup>. The proposed procedure requires first aligning the whole pelvis,  
88 using four landmarks; the authors propose a procedure to dissect the specimen to obtain  
89 two hemipelvises which preserve the same alignment previously identified for the whole  
90 pelvis. The requirement of a whole pelvis as a starting point may be a limitation, as  
91 sometimes only hemipelvic specimens are available.

92 The aims of the present study were to:



- 93 1. Define a reference frame for human hemipelvis that relies on robust anatomical  
94 landmarks and is suitable for *in vitro* applications.
- 95 2. Identify the alignment of the hemipelvis based on the alignment of a whole pelvis.  
96 This includes investigating differences in alignment between right and left, and  
97 between male and female.
- 98 3. Identify the relative alignment of the newly proposed *in vitro* reference frame with  
99 respect to the reference frame usually adopted in gait analysis <sup>4</sup>.
- 100 4. Create an *in vitro* alignment procedure for hemipelvic specimens easy, robust and  
101 inexpensive.
- 102 5. Quantify the intra-operator repeatability and inter-operator reproducibility of the  
103 proposed procedure.

## 104 **2. MATERIAL AND METHODS**

105 An overview of the workflow is provided in Fig. 1. A practical *in vitro* identification of  
106 suitable pelvic landmarks was created. Computed tomography (CT) scans of human  
107 pelvises were analyzed to identify the alignment of selected landmarks of the hemipelvis  
108 with respect to the whole pelvis. An *in vitro* alignment procedure was developed for  
109 human hemipelvic specimens. The intra-operator repeatability and the inter-operator  
110 reproducibility of the procedure were measured.

## 111 **2.1 *In vitro* identification of the landmarks**

112 As shown in different areas, identification of landmarks by palpation leaves a large  
113 uncertainty and subjectivity<sup>34</sup>. Direct *in vitro* identification of the landmarks can be more  
114 accurate and precise. In order to implement a reproducible procedure, a robust method to  
115 identify landmarks, suitable both for pelvis and hemipelvis, was adapted from those  
116 commonly used *in vivo*<sup>4</sup> (Fig. 2):

- 117 • The iliac and pubic regions must be brought in contact with a plane, while the iliac  
118 wing is vertical. ASIS is found as the most external point of the iliac crest, which  
119 is in contact against the plane.
- 120 • With the bone in the same position, PT is found as the point on the pubic tubercle  
121 region, which is in contact against the plane.
- 122 • The iliac and ischial regions must be brought in contact with a plane while the iliac  
123 wing is vertical. PSIS is found as the most external point of the iliac wing, which  
124 is in contact against the plane.

## 125 **2.2 Identification of the anatomical alignment of the hemipelvis based on the** 126 **alignment of the whole pelvis, and comparison with ISB frame**

127 In order to adapt to a single hemipelvis the reference frame based on the APP (which is  
128 defined for an whole pelvis), the alignment of the hemipelvis relative to the alignment of  
129 its respective whole pelvis was identified. Furthermore, the relative orientation of the  
130 proposed reference frame with respect to a reference frame commonly used in gait  
131 analysis<sup>4</sup> was measured based on the same landmarks. To the Authors' knowledge, this is

132 the first time that similar analysis was made to overcome limitations related to other  
133 alignments such as those based on the acetabular plane.

### 134 **2.2.1 Analysis of patient CT scans**

135 Fifty-three CT scans were randomly selected among those taken for hip patients at Istituto  
136 Ortopedico Rizzoli between 2014 and 2017. The patients were 25 male and 28 female,  
137 27-88 years old. The scans had a voxel size of 0.7-0.8 mm. The scans were imported and  
138 analyzed through nmsBuilder v1.0<sup>35</sup>. For each scan, the landmarks (ASIS, PSIS and PT)  
139 were identified on the whole pelvis according to the description above. The pelvises were  
140 oriented in order to reach the ANP (tolerance 0.1 degrees). To measure the alignment of a  
141 single hemipelvis relative to the alignment of its respective whole pelvis, two different  
142 angles were measured (Fig. 3):

- 143 •  $\beta$ : the angle formed by the line connecting PT and ASIS with the transverse plane  
144 of the whole pelvis;
- 145 •  $\delta$ : the angle formed by the line connecting ASIS and PSIS with the sagittal plane  
146 of the whole pelvis.

147 In addition, the relative orientation of the proposed reference frame with respect to the ISB  
148 reference frame<sup>4</sup> (which is commonly used in gait analysis) was measured in all scans  
149 after identifying the mid-point of the two PSIS (mid PSISs): this consisted in a single  
150 rotation ( $\xi$ ), in a sagittal plane (Fig. 3).

151 To exclude outliers, Peirce's criterion was applied<sup>36;37</sup>. Suspect data were checked  
152 among subjects, for both angles. To test the procedure, three skilled operators processed

153 three CT scans three time each. To avoid any bias, the scan elaboration was performed on  
154 different days between repetitions, so that the operator could not recognize previous  
155 elaborations. To assess the intra-operator repeatability (i.e. when the same operator  
156 repeatedly elaborates the same CT scan), the standard deviation between the three  
157 repetitions was computed, for each of the operators and each CT scan. The repeatability  
158 was computed as the root-mean-square-average between CT scans and operators. To  
159 assess the inter-operator reproducibility (i.e. when different operators elaborate the same  
160 CT scan), for each of the operators and each CT scan, the average value was computed out  
161 of three repetitions. The reproducibility was computed as the standard deviation between  
162 the operators.

163 The significance of differences between the right and left hemipelvises was tested with a  
164 paired t-test for  $\beta$  and  $\delta$ . Differences between male and female for  $\beta$  and  $\delta$  were tested  
165 with an unpaired t-test. A threshold of  $p=0.05$  was assumed. Statistical analyses were  
166 performed using MatLab (2009 Edition, MathWorks, Natick, MA, USA).

### 167 **2.3 Alignment procedure for the human hemipelvis**

168 In order to separately control the rotations, the hemipelvises were equipped with a  
169 dedicated handle, which was clamped in a 6-degrees of freedom manipulator. The first  
170 part of the procedure required aligning the landmarks with respect to horizontal and  
171 vertical planes (Fig. 4):

- 172 • Vertical adjustment: the three landmarks were positioned at the same height (i.e.  
173 using an adjustable plate and plasticine);

174       • Horizontal adjustment: ASIS and PT were positioned parallel to the edge of the  
175       reference plane.

176   At this point the hemipelvis had a known alignment. To overcome the limitations of  
177   defining the acetabular plane based on the acetabular rim <sup>30</sup>, a *standard acetabular plane*  
178   was defined (SAP, see Appendix I). With the aim of aligning the hemipelvis with the  
179   SAP horizontal, the specimen was subsequently rotated by two angles (Fig. 5) (see  
180   Appendix I):

181       • Rotation in the posterior direction by  $\Phi = 51^\circ$ ;

182       • Rotation in the medial direction by  $\Omega = 10^\circ$ .

## 183   **2.4 Assessment of the intra-operator repeatability and inter-operator** 184   **reproducibility**

185   To test the alignment procedure, hemipelvic bone specimens in solid foam (ERP  
186   Mod.1291, ERP Mod.1294, Sawbones, Malmö, Sweden) were adopted. In order to  
187   measure the alignment achieved, a squared plastic block was rigidly fixed on the  
188   hemipelvises; the absolute orientation of its faces was measured, after the alignment,  
189   through a goniometer (Art. 06.07503, IDF, Pontoglio (BS), Italy; precision: 0.1 degrees).

190   Four operators aligned the two specimens three times each. In order to evaluate the  
191   robustness of the procedure two skilled operators (who performed at least one alignment  
192   procedure) and two inexperienced operators were chosen. To avoid any bias, the  
193   specimen orientation was modified between repetitions. To assess the intra-operator  
194   repeatability, the standard deviation between the three repetitions was computed, for each

195 of the operators and each specimen. The repeatability was computed as the root-mean-  
196 square-average between specimens and operators. To assess the inter-operator  
197 reproducibility, for each of the operators and each specimen, the average value was  
198 computed, out of three repetitions. The reproducibility was computed as the standard  
199 deviation between the operators. Statistical analyses were performed using MatLab (2009  
200 Edition, MathWorks, Natick, MA, USA).

### 201 **3. RESULTS**

#### 202 **3.1 Alignment of hemipelvis based on the alignment of whole pelvis**

203 The landmarks could be easily identified in all the CT scans. Based on the Peirce's  
204 criterion, five cases were excluded for  $\beta$  and none for  $\delta$ . The intra-operator repeatability  
205 was below  $0.6^\circ$  for  $\beta$ , and below  $0.5^\circ$  for  $\delta$ . The inter-operator reproducibility was better  
206 than  $\pm 2.6^\circ$  for  $\beta$  and better than  $\pm 3.8^\circ$  for  $\delta$ .

207 The difference between right and left hemipelvises was on average  $0.3^\circ$  for  $\beta$  ( $p > 0.7$ ) and  
208  $0.2^\circ$  for  $\delta$  ( $p > 0.7$ ). In none of the 53 pelvises examined, a difference greater than  $9^\circ$  was  
209 observed between the left and right hemipelvis for  $\beta$  and  $\delta$ . The values of  $\beta$  in the female  
210 subjects were  $0.6^\circ$  larger than for the males, but this difference was not statistically  
211 significant ( $p = 0.4$ , Table 1). The values of  $\delta$  were  $0.1^\circ$  larger for the female subjects than  
212 for the males ( $p = 0.9$ , Table 1). The relative orientation of the proposed reference frame  
213 with respect to the ISB reference frame in the sagittal plane was on average  $\xi = 10.7^\circ$ . The  
214 difference between male and female for  $\xi$  was  $0.6^\circ$  and not statistically significant ( $p = 0.6$ ,  
215 Table 1).

### 216 **3.2 Alignment procedure**

217 All operators performed successfully the alignment, for all the specimens. The time  
218 required was about 15 minutes for each specimen. The intra-operator repeatability was  
219 generally below  $1.5^\circ$  for each angle (Fig. 6). The inter-operator reproducibility was less  
220 than  $\pm 2.0^\circ$  for each angle. Alignment in the transverse plane was most repeatable.

## 221 **4. DISCUSSION**

222 The aim of this study was to define a reference frame suitable for *in vitro* biomechanical  
223 testing of the human pelvis, based on robust anatomical landmarks. As *in vitro* tests are  
224 often performed on hemipelvises, the procedure was devised for a hemipelvis (rather than  
225 relying on a whole pelvis). To enable comparisons and registrations with other studies,  
226 the alignment with respect to a reference frame commonly used in movement analysis was  
227 measured. Finally, we aimed at evaluating the reliability of the protocol in terms of intra-  
228 operator repeatability and inter-operator reproducibility.

229 The alignment protocol revolved around anatomical landmarks, which could be accurately  
230 identified on the physical *in vitro* specimens. The analysis of 53 patients' CT scans  
231 allowed identifying the average alignment of a hemipelvis based on the alignment of its  
232 original whole pelvis. No significant differences were detected between right and left  
233 sides and between male and female specimens. Furthermore, the relative alignment of the  
234 newly proposed *in vitro* reference frame for the hemipelvis was measured with respect to a  
235 reference frame commonly used in gait analysis<sup>4</sup>. Thus, even if the rationale of this study  
236 drove us to choose a different reference frame, it is possible to refer our *in vitro* frame to  
237 the one used in gait analysis.

238 When the landmarks were identified *in silico* on CT scans, the intra-operator repeatability  
239 was 0.5° in the frontal plane, and 0.5° in the transverse plane; the inter-operator  
240 reproducibility was 2.6° in the frontal plane and 3.8° in the transverse plane. When the  
241 alignment procedure was applied to physical hemipelvises *in vitro*, the intra-operator  
242 repeatability was generally below 1.5°, and the inter-operator reproducibility was less than  
243 ±2.0°. The variability mainly depends on the uncertainty in the identification of the  
244 landmarks. Due to the limited resolution of the CT scans, it is not surprising that the  
245 uncertainty of the *in silico* alignment was worse than the *in vitro* one.

246 Past studies, where a reference frame was defined for other bone segments (tibia <sup>6</sup>, and  
247 vertebra <sup>5</sup>), reported errors of the order of 1°-3°, comparable to the present one. Only few  
248 studies expressly defined a reference frame for the human pelvis *in vitro* <sup>22-26; 31; 38</sup>.

249 Comparisons with the present study are difficult, as the reproducibility of such references  
250 has only seldom been quantified. For instance, Anderson *et al.* performed an *in vitro*  
251 alignment of a whole pelvis based on the ASIS and pubic symphysis: while they focused  
252 on relative rotations, they did not report the accuracy of their original alignment <sup>39</sup>. A  
253 reference frame based on the acetabular plane is often adopted for *in vitro* purposes <sup>24-26;</sup>  
254 <sup>31</sup>. However, identification of this plane is complex due to the irregular shape of the  
255 acetabular rim <sup>32; 33</sup>. To overcome this problem, we defined the alignment for a standard  
256 acetabular plane (SAP) based on the advice of a group of hip surgeons.

257 To the Authors' knowledge, this is the second study in which a reference frame for the  
258 hemipelvis was derived from the reference frame of the whole pelvis. In fact, van Arkel *et*  
259 *al.* developed a procedure to apply the ISB reference frame to the whole pelvis before  
260 bisecting it, and then apply the same reference when the hemipelvises were used for *in*



261 *vitro* testing<sup>4;22</sup>. They found that after bisection, the hemipelvis had a misalignment  
262 compared to the original whole pelvis. The error was  $1.5\pm 1.6^\circ$  for the adduction,  $0.5\pm 1.1^\circ$   
263 for the internal rotation, and  $0.6\pm 1.7^\circ$  for the flexion. However, as this error does not  
264 include the intra- and inter-operator uncertainty in identifying the landmarks and initially  
265 aligning the whole pelvis, the resultant total error of their procedure is larger (i.e. the sum  
266 of such errors, and of the uncertainties in aligning the whole pelvis). Furthermore, for  
267 some applications it might be preferable not to drill the large screw holes required to hold  
268 the specimen during bisection<sup>22</sup>.

269 The main limitation of our approach is probably that, in order to standardize the reference  
270 frame, and to be able to implement it on isolated hemipelvises, we were forced to make a  
271 number of simplifications such as applying to any specimen the same average values of  
272 the angles. We assumed that the anterior pelvic plane was vertical. However, the inter-  
273 subject variability has been reported due to patient's anatomy and pose (i.e. when  
274 changing from supine to standing position)<sup>40;41</sup>. Consistently with our aim of  
275 standardizing the alignment procedure, we assigned the alignment that corresponds to the  
276 average reported in the literature (around  $0^\circ$ <sup>21;41;42</sup>). Similarly, the alignment of the  
277 standard acetabular plane was defined based on angle values agreed upon by a pool of  
278 surgeons. In principle, the proposed alignment procedure can be implemented also with  
279 different angles for the acetabular plane: one just needs to change the final couple of  
280 rotations.

281 The procedure has been tested on synthetic models of the pelvis. To include the  
282 variability, both male and female specimens were used. Such models provide detailed

283 anatomy, including the presence and shape of the landmarks. This allowed testing the  
284 intra-operator repeatability and inter-operator reproducibility of the alignment procedure.

285 An *in vitro* implementation of a procedure to identify robust anatomical landmarks allows  
286 objectively determine the reference points for the alignment. It is important to underline  
287 that reproducibility and repeatability of an alignment procedure strongly depend on the  
288 identification of the anatomical landmarks; hence practical rules to identify these  
289 landmarks should be always taken in consideration for *in vitro* purposes. The reference  
290 frame and alignment procedure developed can be applied each time a hemipelvic  
291 specimen is studied, both *in vitro* and *in silico*. Furthermore, the proposed reference  
292 frame can be easily registered to match a reference frame commonly used in gait analysis.  
293 Moreover, the intra-operator repeatability and inter-operator reproducibility quantified in  
294 the present study are sufficient for most *in vitro* applications. For these reasons, the  
295 presented procedure to align hemipelvic specimens is sufficiently robust, standardized,  
296 and accessible, hence can be easily replicated in other laboratories. The proposed  
297 reference frame can therefore be assumed as a starting point for numerous pre-clinical *in*  
298 *vitro* tests e.g. to test implant stability of acetabular reconstructions.

299

## 300 **APPENDIX I: Standard acetabular plane (SAP)**

301 To overcome the known uncertainties and limitations of defining the acetabular plane  
302 based on the acetabular rim <sup>30</sup>, a *standard acetabular plane* was defined (SAP). Standard  
303 values for acetabular inclination (45 degrees) and anteversion (20 degrees) were chosen  
304 according to a pool of experienced hip surgeons. Both values are within the Lewinnek  
305 “safe zone” (inclination =  $40^{\circ} \pm 10^{\circ}$ ; anteversion =  $15^{\circ} \pm 10^{\circ}$ ) <sup>17</sup>, which represents the goal  
306 for most surgeons during cup implantation <sup>17; 19; 43; 44</sup>. It was demonstrated that prosthesis  
307 implanted within the “safe zone” better resist to dislocation and impingement <sup>17; 45</sup>.

308 The angles necessary to align the SAP horizontal were calculated combining the  
309 alignment of the hemipelvis based on the whole pelvis, and the inclination and anteversion  
310 of the SAP (Fig. 7):

- 311 • Rotation in a quasi-transverse plane:

$$312 \quad \Phi = \text{Acetabular anteversion} + \delta = 20^{\circ} + 31^{\circ} = 51^{\circ}$$

- 313 • Rotation in the frontal plane:

$$314 \quad \Omega = \text{Acetabular inclination} - \beta = 45^{\circ} - 35^{\circ} = 10^{\circ}$$

315 where:

- 316 •  $\beta$  and  $\delta$  are the average values of the angles measured from the 53 CT scans, to  
317 align the hemipelvis based on the whole pelvis (see Par. 3.1).
- 318 •  $\Phi$  and  $\Omega$  are the final angles to align the hemipelvis with the SAP horizontal.
- 319 • All values were rounded to the closest integer.

320 **Acknowledgments**

321 The Authors wish to thank Aesculap AG Research & Development for the financial  
322 support. The authors gratefully acknowledge the advice of the pool of hip surgeons,  
323 namely Prof. Vollkmar Jansson, Prof. Maximilian Rudert, Prof. Heiko Graichen and Prof.  
324 Cesare Faldini.

325

326 **REFERENCES**

- 327 1. Cappozzo A, Catani F, Croce UD, et al. 1995. Position and orientation in space of  
328 bones during movement: anatomical frame definition and determination. Clin  
329 Biomech (Bristol, Avon) 10:171-178.
- 330 2. Wu G, Cavanagh PR. 1995. ISB recommendations for standardization in the  
331 reporting of kinematic data. J Biomech 28:1257-1261.
- 332 3. Cristofolini L. 2012. Anatomical reference frames for long bones: biomechanical  
333 applications. In: Preedy VRE editor. Handbook of Anthropometry: Physical  
334 Measures of Human Form In Health and Disease. New York: Springer.
- 335 4. Wu G, Siegler S, Allard P, et al. 2002. ISB recommendation on definitions of joint  
336 coordinate system of various joints for the reporting of human joint motion--part I:  
337 ankle, hip, and spine. International Society of Biomechanics. J Biomech 35:543-  
338 548.
- 339 5. Danesi V, Zani L, Scheele A, et al. 2014. Reproducible reference frame for in vitro  
340 testing of the human vertebrae. J Biomech 47:313-318.
- 341 6. Conti G, Cristofolini L, Juszczuk M, et al. 2008. Comparison of three standard  
342 anatomical reference frames for the tibia-fibula complex. J Biomech 41:3384-  
343 3389.
- 344 7. Clohisy JC, Carlisle JC, Beaulé PE, et al. 2008. A systematic approach to the plain  
345 radiographic evaluation of the young adult hip. J Bone Joint Surg Am 90 Suppl  
346 4:47-66.
- 347 8. Shon WY, Gupta S, Biswal S, et al. 2008. Validation of a simple radiographic  
348 method to determine variations in pelvic and acetabular cup sagittal plane  
349 alignment after total hip arthroplasty. Skeletal Radiol 37:1119-1127.

- 350 9. Tannast M, Murphy SB, Langlotz F, et al. 2006. Estimation of pelvic tilt on  
351 anteroposterior X-rays--a comparison of six parameters. *Skeletal Radiol* 35:149-  
352 155.
- 353 10. Sotereanos NG, Miller MC, Smith B, et al. 2006. Using intraoperative pelvic  
354 landmarks for acetabular component placement in total hip arthroplasty. *J*  
355 *Arthroplasty* 21:832-840.
- 356 11. Bergmann G, Deuretzbacher G, Heller M, et al. 2001. Hip contact forces and gait  
357 patterns from routine activities. *J Biomech* 34:859-871.
- 358 12. Wan Z, Malik A, Jaramaz B, et al. 2009. Imaging and navigation measurement of  
359 acetabular component position in THA. *Clin Orthop Relat Res* 467:32-42.
- 360 13. Digioia AM, Jaramaz B, Plakseychuk AY, et al. 2002. Comparison of a  
361 mechanical acetabular alignment guide with computer placement of the socket. *J*  
362 *Arthroplasty* 17:359-364.
- 363 14. DeChenne CL, Jayaram U, Lovell T, et al. 2005. A novel acetabular alignment  
364 guide for THR using selective anatomic landmarks on the pelvis. *J Biomech*  
365 38:1902-1908.
- 366 15. Barbier O, Skalli W, Mainard L, et al. 2014. The reliability of the anterior pelvic  
367 plane for computer navigated acetabular component placement during total hip  
368 arthroplasty: prospective study with the EOS imaging system. *Orthop Traumatol*  
369 *Surg Res* 100:S287-291.
- 370 16. Dandachli W, Richards R, Sauret V, et al. 2006. The transverse pelvic plane: a  
371 new and practical reference frame for hip arthroplasty. *Comput Aided Surg*  
372 11:322-326.

- 373 17. Lewinnek GE, Lewis JL, Tarr R, et al. 1978. Dislocations after total hip-  
374 replacement arthroplasties. *J Bone Joint Surg Am* 60:217-220.
- 375 18. Kiefer H. 2003. OrthoPilot cup navigation--how to optimise cup positioning? *Int*  
376 *Orthop* 27 Suppl 1:S37-42.
- 377 19. Nogler M, Kessler O, Prassl A, et al. 2004. Reduced variability of acetabular cup  
378 positioning with use of an imageless navigation system. *Clin Orthop Relat*  
379 *Res*:159-163.
- 380 20. Kendall FP, McCreary EK, Provance PG. 1993. *Muscles, Testing and Function:*  
381 *With Posture and Pain*, 4th ed. Baltimore;
- 382 21. Loppini M, Longo UG, Ragucci P, et al. 2016. Analysis of the Pelvic Functional  
383 Orientation in the Sagittal Plane: A Radiographic Study With EOS 2D/3D  
384 Technology. *J Arthroplasty*.
- 385 22. van Arkel RJ, Jeffers JR. 2016. In vitro hip testing in the International Society of  
386 Biomechanics coordinate system. *J Biomech* 49:4154-4158.
- 387 23. Lewton KL. 2015. In vitro bone strain distributions in a sample of primate pelvis.  
388 *J Anat* 226:458-477.
- 389 24. Zant NP, Wong CK, Tong J. 2007. Fatigue failure in the cement mantle of a  
390 simplified acetabular replacement model. *Int J Fatigue* 29:1245-1252.
- 391 25. Wang JY, Heaton-Adegbile P, New A, et al. 2009. Damage evolution in acetabular  
392 replacements under long-term physiological loading conditions. *J Biomech*  
393 42:1061-1068.
- 394 26. Heaton-Adegbile P, Zant NP, Tong J. 2006. In vitro fatigue behaviour of a  
395 cemented acetabular reconstruction. *J Biomech* 39:2882-2886.

- 396 27. Preece SJ, Willan P, Nester CJ, et al. 2008. Variation in pelvic morphology may  
397 prevent the identification of anterior pelvic tilt. *J Man Manip Ther* 16:113-117.
- 398 28. Malik A, Wan Z, Jaramaz B, et al. 2010. A validation model for measurement of  
399 acetabular component position. *J Arthroplasty* 25:812-819.
- 400 29. Józwiak M, Rychlik M, Musielak B, et al. 2015. An accurate method of  
401 radiological assessment of acetabular volume and orientation in computed  
402 tomography spatial reconstruction. *BMC Musculoskelet Disord* 16:42.
- 403 30. Murray DW. 1993. The definition and measurement of acetabular orientation. *J*  
404 *Bone Joint Surg Br* 75:228-232.
- 405 31. Tong J, Zant NP, Wang JY, et al. 2008. Fatigue in cemented acetabular  
406 replacements. *Int J Fatigue* 30:1366-1375.
- 407 32. Wada H, Mishima H, Yoshizawa T, et al. 2016. Initial Results of an Acetabular  
408 Center Axis Registration Technique in Navigated Hip Arthroplasty with Deformed  
409 Acetabular Rims. *Open Orthop J* 10:26-35.
- 410 33. Vandebussche E, Saffarini M, Taillieu F, et al. 2008. The asymmetric profile of  
411 the acetabulum. *Clin Orthop Relat Res* 466:417-423.
- 412 34. Mieritz RM, Kawchuk GN. 2016. The Accuracy of Locating Lumbar Vertebrae  
413 When Using Palpation Versus Ultrasonography. *J Manipulative Physiol Ther*  
414 39:387-392.
- 415 35. Valente G, Pitto L, Testi D, et al. 2014. Are subject-specific musculoskeletal  
416 models robust to the uncertainties in parameter identification? *PLoS One*  
417 9:e112625.
- 418 36. Peirce B. 1852. Criterion for the rejection of doubtful observations. *Astronomical*  
419 *Journal* 2:161-163.



- 420 37. Ross SM. 2003. Peirce's criterion for the elimination of suspect experimental data.  
421 Journal of Engineering Technology 20:38-41.
- 422 38. Zant NP, Heaton-Adegbile P, Hussell JG, et al. 2008. In vitro fatigue failure of  
423 cemented acetabular replacements: a hip simulator study. J Biomech Eng  
424 130:021019.
- 425 39. Anderson AE, Ellis BJ, Maas SA, et al. 2008. Validation of finite element  
426 predictions of cartilage contact pressure in the human hip joint. J Biomech Eng  
427 130:051008.
- 428 40. Pinoit Y, May O, Girard J, et al. 2007. [Low accuracy of the anterior pelvic plane  
429 to guide the position of the cup with imageless computer assistance: variation of  
430 position in 106 patients]. Rev Chir Orthop Reparatrice Appar Mot 93:455-460.
- 431 41. DiGioia AM, Hafez MA, Jaramaz B, et al. 2006. Functional pelvic orientation  
432 measured from lateral standing and sitting radiographs. Clin Orthop Relat Res  
433 453:272-276.
- 434 42. Blondel B, Parratte S, Tropiano P, et al. 2009. Pelvic tilt measurement before and  
435 after total hip arthroplasty. Orthop Traumatol Surg Res 95:568-572.
- 436 43. Nogler M, Mayr E, Krismer M, et al. 2008. Reduced variability in cup positioning:  
437 the direct anterior surgical approach using navigation. Acta Orthop 79:789-793.
- 438 44. Opperer M, Lee YY, Nally F, et al. 2016. A critical analysis of radiographic  
439 factors in patients who develop dislocation after elective primary total hip  
440 arthroplasty. Int Orthop 40:703-708.
- 441 45. Barrack RL. 2003. Dislocation after total hip arthroplasty: implant design and  
442 orientation. J Am Acad Orthop Surg 11:89-99.

443

444 **TABLES**

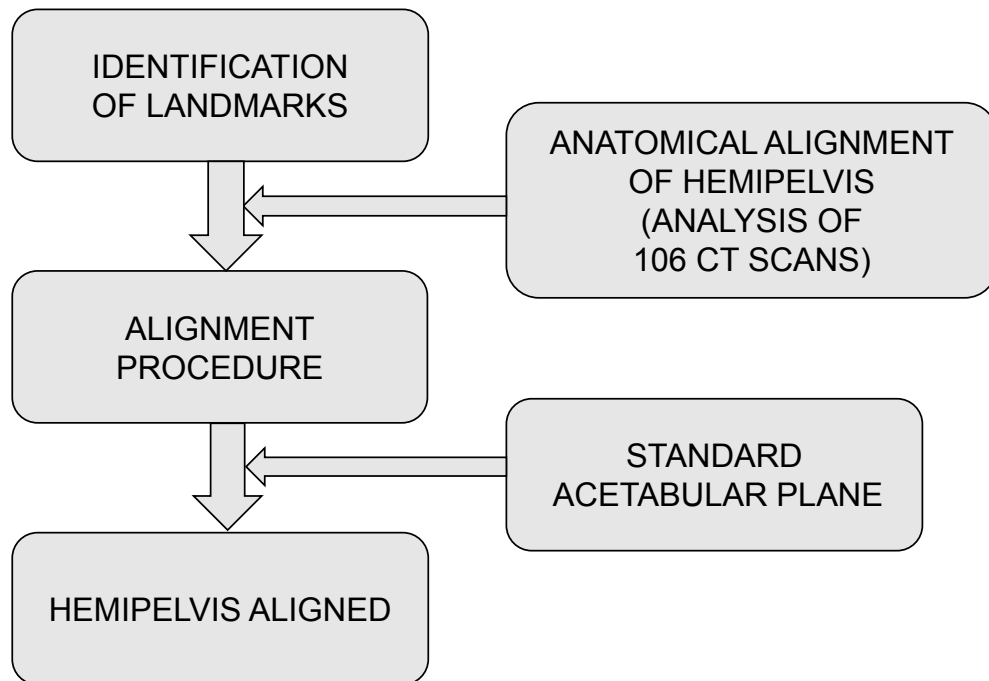
445 **Table 1** – Values of  $\beta$ ,  $\delta$  and  $\xi$  measured in the CT scans of 53 subjects (Fig. 3). Average  
 446 and standard deviation are reported, after excluding outliers, for all subjects, and split by  
 447 gender. The last column shows the average difference, and statistical significance  
 448 (unpaired t-test).

Angles	All	Male	Female	Difference between Male and Female
$\beta$	$35.5^\circ \pm 4.0^\circ$	$35.2^\circ \pm 4.9^\circ$	$35.9^\circ \pm 2.6^\circ$	$0.6^\circ$ ( $p=0.4$ )
$\delta$	$31.3^\circ \pm 3.8^\circ$	$31.4^\circ \pm 3.8^\circ$	$31.3^\circ \pm 3.9^\circ$	$0.1^\circ$ ( $p=0.9$ )
$\xi$	$10.7^\circ \pm 5.8^\circ$	$11.0^\circ \pm 6.2^\circ$	$10.3^\circ \pm 5.4^\circ$	$0.6^\circ$ ( $p=0.6$ )

449

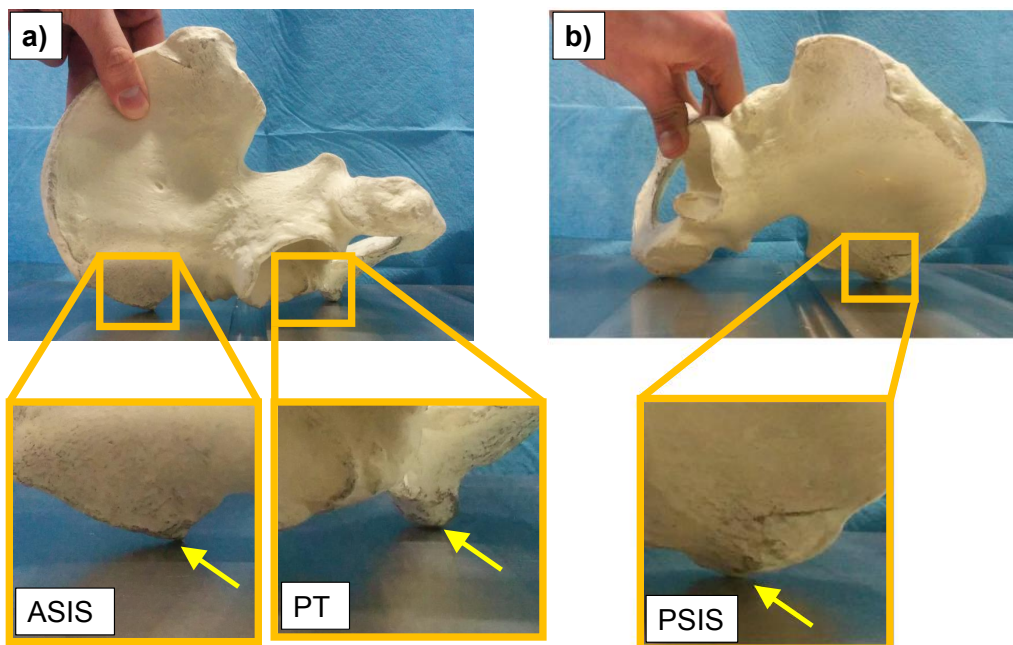
450

451 **CAPTIONS TO FIGURES**



452

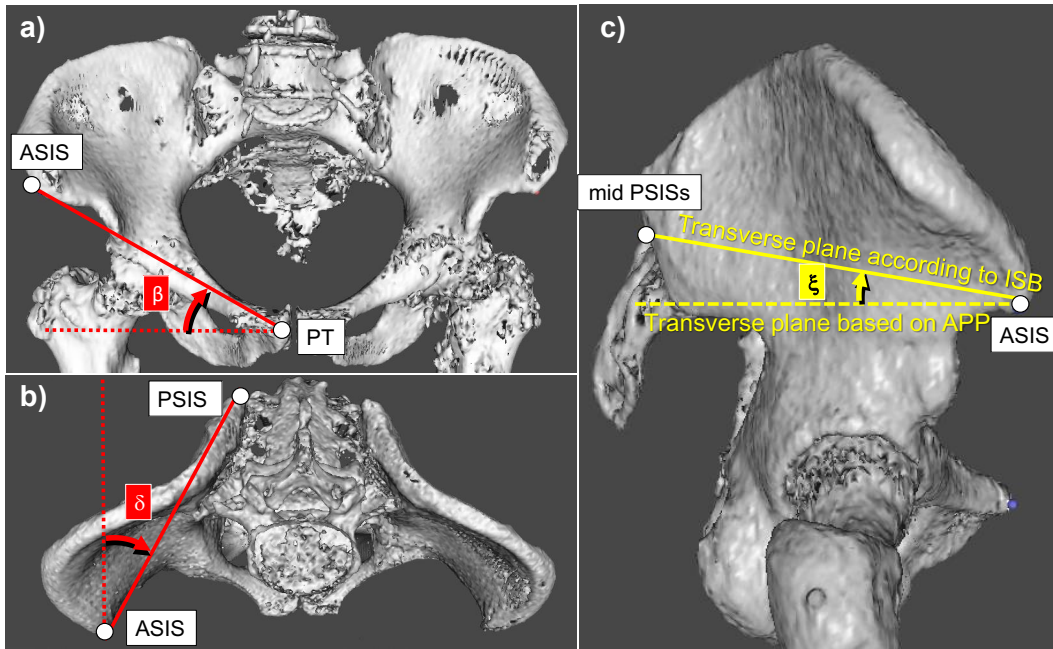
453 **Fig. 1** - Workflow of the proposed alignment procedure for the hemipelvis.



454

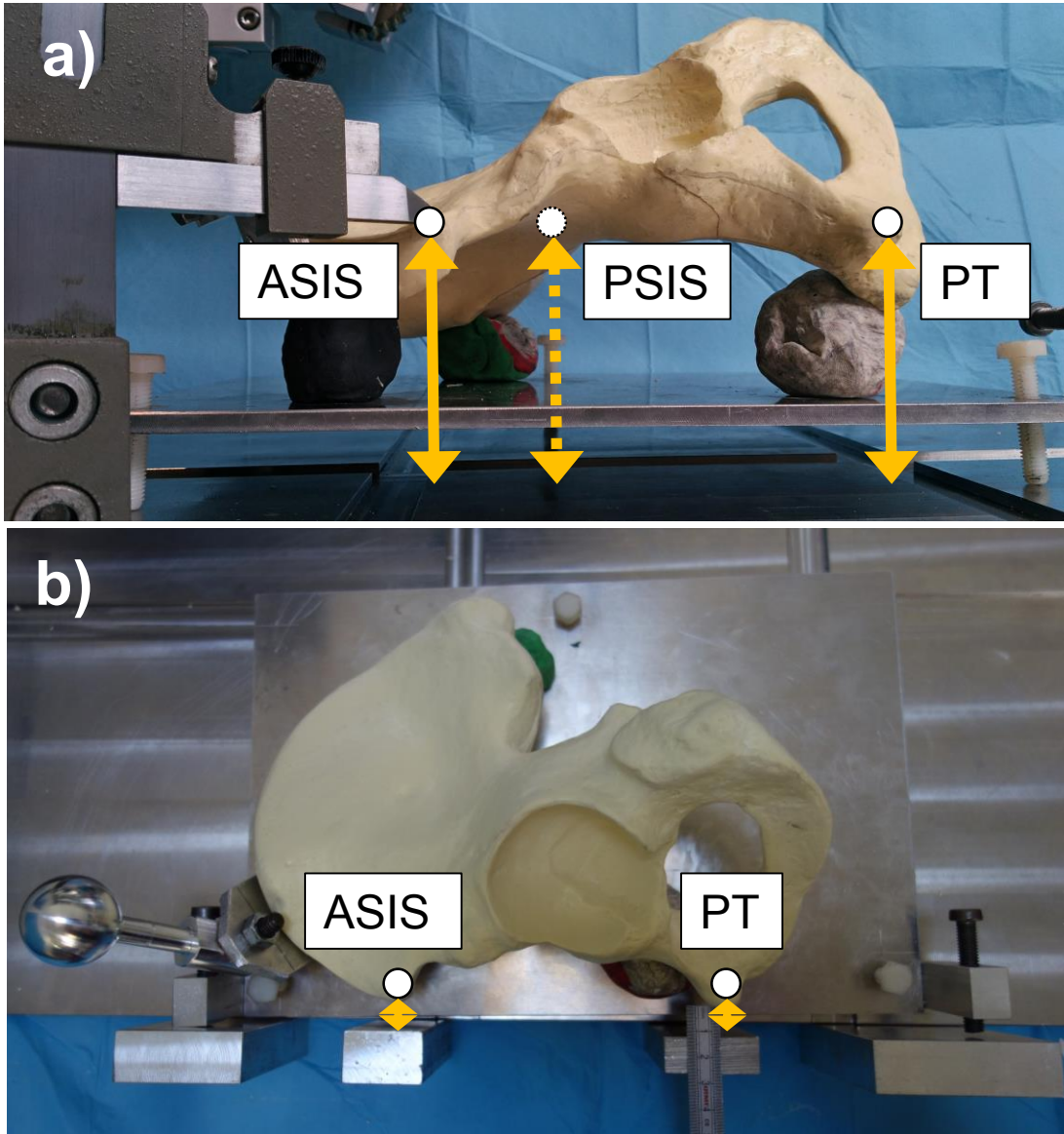
455 **Fig. 2** - *In vitro* identification of the landmarks on a hemipelvis: a) ASIS and PT, b) PSIS.

456 A left specimen is shown in these pictures.



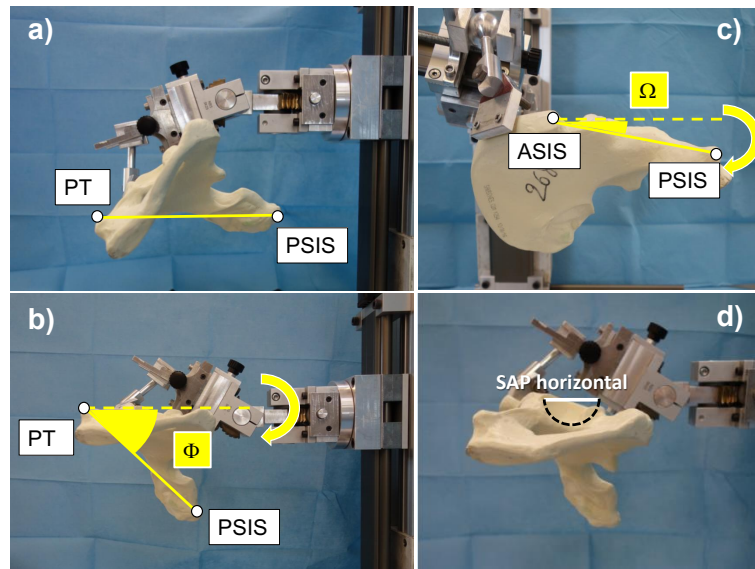
457  
458

**Fig. 3** - Three different angles were measured in the 53 patient CT scans using  
 459 nmsBuilder. a) The angle ( $\beta$ ) formed by the line connecting PT and ASIS with the  
 460 transverse plane of the whole pelvis was measured in a frontal view. b) The angle ( $\delta$ )  
 461 formed by the line connecting ASIS and PSIS with the sagittal plane of the whole pelvis  
 462 was measured in a transverse plane. c) The angle ( $\xi$ ) between the proposed reference  
 463 frame (based on the APP) and the ISB reference frame was measured in a lateral view.



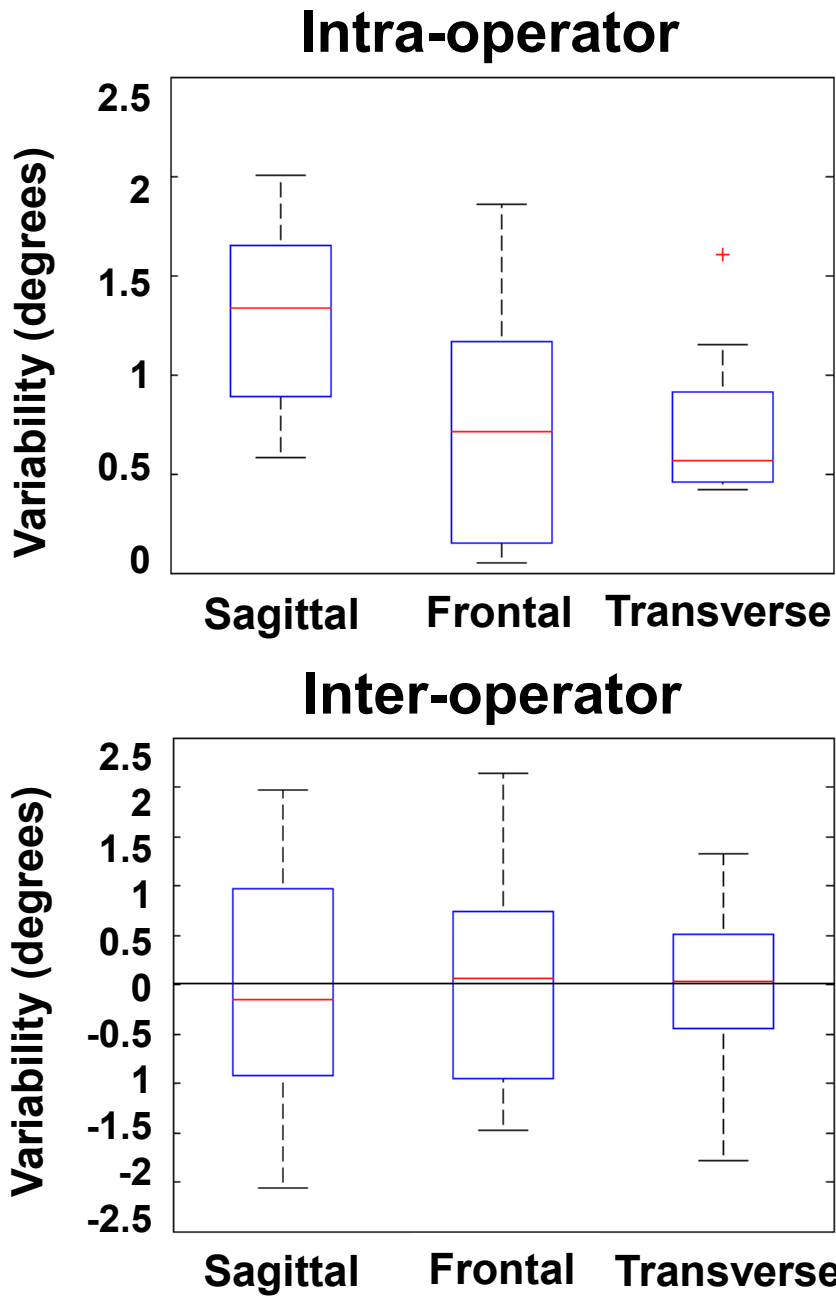
464

465 **Fig. 4** – Alignment of a left hemipelvis: a) Vertical adjustment of the three landmarks.  
 466 Quasi-frontal view, with the ASIS, PT and PSIS (hidden by the hemipelvis) at the same  
 467 height, as measured with the vertical ruler (visible in the far left of the picture). Also  
 468 visible is the spherical handle mounted on the hemipelvis. b) Horizontal adjustments of  
 469 the landmarks. Lateral view of a left hemipelvis with ASIS and PT aligned with the edge  
 470 of the reference plane.



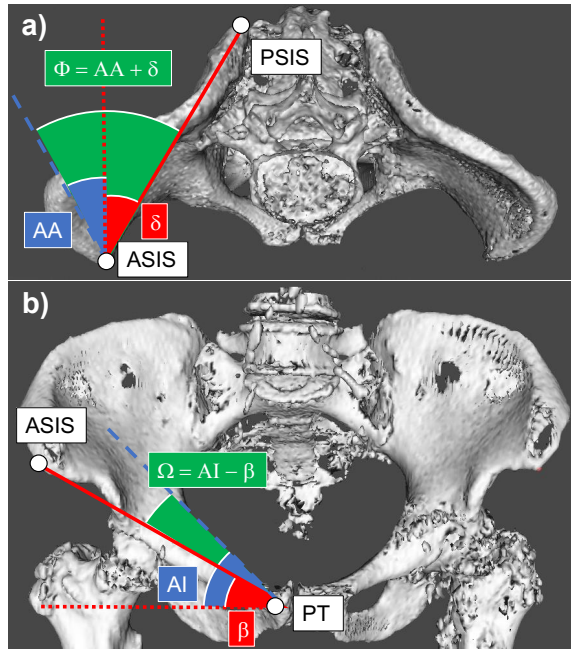
471

472 **Fig. 5** – Hemipelvis clamped in the 6-degrees of freedom manipulator through the handle  
 473 rigidly fixed to the bone. a) Left hemipelvis viewed from distally (i.e. in a quasi-  
 474 transverse plane) aligned as in Fig. 4, and lifted from the plane. b) Rotation of the  
 475 specimen by  $\Phi$  in the medial direction. c) Rotation of the specimen by  $\Omega$  in the anterior  
 476 direction. d) The standard acetabular plane (SAP) is horizontal once the specimen is  
 477 aligned.



478

479 **Fig. 6** - Variability of measured angles on the hemipelvic specimens in each plane: intra-  
 480 operator repeatability (top) and inter-operator reproducibility (bottom). The red mark  
 481 indicates the median; the blue boxes includes the 25<sup>th</sup> –75<sup>th</sup> percentile; the whiskers extend  
 482 to the most extreme data points. The outliers are marked with red crosses, and were  
 483 excluded from the analysis.



484

485 **Fig. 7** – Combination of angles to align a hemipelvis with the standard acetabular plane  
 486 (SAP) horizontal: (a) Top view of a CT scan of human pelvis showing the angle ( $\Phi$ ),  
 487 which is calculated as the sum between the angle corresponding to the acetabular  
 488 anteversion ( $AA$ ) and  $\delta$ ; (b) Frontal view showing the angle ( $\Omega$ ), which is calculated as the  
 489 difference between the angle corresponding to the acetabular inclination ( $AI$ ) and  $\beta$ .