



In-house three dimensional-printed cutting guides improve surgical accuracy in children who underwent resection of malignant bone tumours of lower limb and reconstruction with allograft

Eiji Nakata^{1,2} · Giulia Alessandri³ · Grazia Chiara Menozzi³ · Ayano Aso² · Toshifumi Ozaki¹ · Giovanni Trisolino³ · Davide Maria Donati² · Costantino Errani²

Received: 28 January 2026 / Accepted: 5 March 2026 / Published online: 17 March 2026
© The Author(s) 2026

Abstract

Aims This study evaluated the accuracy of resection of bone tumours and the fit between host bone and massive bone allograft (MBA) in children with malignant bone tumours of lower limb who underwent surgery using in-house 3-dimensional (3D)-printed patient-specific instruments (PSIs) for tumour resection and graft-specific instruments (GSIs) for shaping the MBA.

Methods This retrospective study included seven children (3 males, 4 females; median age 13) with malignant bone tumours of the lower limb who underwent intercalary resection and reconstruction with MBA between September 2023 and March 2025 using in-house designed 3D-printed PSIs and GSIs. Tumours were located in the femur (5 children) and tibia (2 children). We analysed the accuracy of bone resection, complications of reconstruction, and function of patients.

Results All resections achieved R0 margins. The median planned resection length was 16.5 cm versus 16.8 cm actually resected (median difference 0.2 cm). Bone union was achieved in 13 of 14 (92.9%) osteotomy sites. Bone union was faster at metaphyseal junctions (median 5.9 months) than diaphyseal junctions (median 8.4 months) ($p=0.01$). One of the osteotomy sites (7.1%) had a delayed union requiring secondary bone grafting. The median Musculoskeletal Tumour Society score was 30 at the last follow-up.

Conclusion 3D-printed PSIs and GSIs appear to enhance the accuracy of bone tumour resection and host bone-MBA fit, thereby reducing the risks of inadequate margins and non-union, respectively.

Keywords Massive bone allograft · In house 3-dimensional-printed patient-specific instruments · Malignant bone tumours · Lower limb · Children

✉ Eiji Nakata
eijinakata8522@yahoo.co.jp

Giulia Alessandri
giulia.alessandri@ior.it

Grazia Chiara Menozzi
graziachiara.menozi@ior.it

Ayano Aso
ayano.aso@studio.unibo.it

Toshifumi Ozaki
tozaki@md.okayama-u.ac.jp

Giovanni Trisolino
giovanni.trisolino@ior.it

Davide Maria Donati
davide.donati@ior.it

Costantino Errani
costantino.errani@ior.it

¹ Department of Orthopedic Surgery, Okayama University Hospital, Okayama city, Japan

² Orthopaedic Service, Musculoskeletal Oncology Department., IRCCS Istituto Ortopedico Rizzoli, Bologna, Italy

³ Unit of Pediatric Orthopedics and Traumatology, IRCCS Istituto Ortopedico Rizzoli, Bologna, Italy

Introduction

Recently, 3-dimensional (3D)-printing technology was clinically applied including the creation of anatomical models, patient-specific cutting guides, and patient-specific prostheses/instruments in the orthopaedic oncological surgery [1–3]. Several retrospective studies showed that 3D-printed PSIs enabled more precise multiplanar osteotomies in complex anatomical locations, such as the pelvis and juxta-articular region, reducing operative time and blood loss [4–7]. Moreover, the use of graft-specific instruments (GSIs) can shape the MBA to adequately match the bone defect following tumour resection [8–10]. Achieving near-perfect congruency between host bone and massive bone allograft (MBA) may increase the contact surface area, which may facilitate bone union [11]. Previous monocentric retrospective studies focusing on the accuracy of bone resection in patients with pelvic and extremity bone tumours using 3D-printed PSIs reported that the difference between the length of preoperatively planned bone resection and the resected specimens ranged from 2.3 mm to 8.4 mm [12]. However, these reports have largely focused on resection accuracy, often in anatomically complex pelvic or juxta-articular locations, and have rarely addressed intercalary reconstructions with MBA, particularly in children [8, 10]. To date no studies reported the accuracy of bone resection and clinical outcome focusing on intercalary resection and reconstruction with MBA using in-house 3D-printed PSIs both for the resection and the reconstruction with MBA in children with malignant bone tumours of lower limb. Therefore, we conducted a retrospective study to evaluate the accuracy of bone resection and reconstruction with MBA following intercalary resection using in-house 3D-printed PSIs in children with malignant lower limb bone tumours, as well as to assess the associated union rates, complications, and functional outcomes.

Materials and methods

Patient characteristics

A retrospective study was conducted on children with malignant bone tumours of the lower limb who underwent intercalary resection of bone tumours and reconstruction with MBA. All children were treated at our institution between September 2023 and March 2025. Inclusion criteria were children with malignant bone tumours of the femur or tibia who underwent intercalary resection and reconstruction with MBA using in-house 3D-printed PSIs and GSIs. Exclusion criteria were adult patients or children who underwent hemi-cortical resection or radiotherapy at the surgical site. During the study period, seven children with malignant bone tumours of the lower limb underwent intercalary resection of the tumour and reconstruction with MBA (Table 1). The patient population consisted of three males and four females, with a median age of 13 years (range 9–17 years). The tumours were located in the femur in five children and in the tibia in two children. Pathological analysis of resected specimens revealed Ewing sarcoma in five children and osteoblastic osteosarcoma in two children. By the American Joint Committee on Cancer staging system, all children were classified as stage IIA. All children received chemotherapy, consisting of a combination of neoadjuvant and adjuvant chemotherapy. Median follow up period was 10.0 months (range 6.2–21.9 months). Surgical margins were evaluated according to the American Joint Committee on Cancer (AJCC) residual tumour classification and categorized as R0 (no residual tumour), R1 (microscopic residual tumour cells at the inked margin), or R2 (macroscopic residual tumour cells) [13].

Table 1 Patient characteristics

Case	Sex	Age at presentation	Location	Diagnosis	Tumor Size (cm)	Length of Planned resection (cm)	Length of resected bone (cm)	Complication	MSTS
1	M	9	Proximal Femur	Ewing sarcoma	3.9	15.6	16	Delayed healing	30
2	M	11	Proximal Femur	Ewing sarcoma	2.9	16.5	16.7	-	30
3	F	17	Distal Femur	Ewing sarcoma	5.2	14.7	15	-	26
4	F	16	Proximal Tibia	Osteosarcoma, osteoblastic	5.1	15	15	-	30
5	M	13	Distal Tibia	Ewing sarcoma	3.1	22	22	-	30
6	F	9	Distal Femur	Osteosarcoma, osteoblastic	4.4	18.5	18.7	-	23
7	F	17	Proximal Femur	Ewing sarcoma	5.2	23.5	23.5	-	29

M male, F female

MSTS musculoskeletal tumour society

Procedure of in-house 3D-printed patient-specific cutting guides

All procedures were planned, simulated, and executed through a close collaboration between the Paediatric Orthopaedics Unit and the Orthopaedic Oncology Unit, within a study protocol approved by the Ethics Committee (NCT05700526). The protocol, which was initially authorized for the management of severe musculoskeletal deformities in paediatric patients, was subsequently amended to include massive resections in paediatric

oncologic cases as well. The in-house 3D-printing workflow is well established and thoroughly validated [14, 15].

Preoperative planning

Preoperative imaging included X-ray, Computed Tomography (CT) scans and Magnetic Resonance Imaging (MRI) to assess bone anatomy and tumour margins (Fig. 1a, b, c) [16]. MRI was utilized to evaluate the extraosseous size and intramedullary extension of the tumour (Fig. 1b, c). CT scans and MRI datasets were segmented to obtain 3D models of bone and tumour tissues and registered to align both

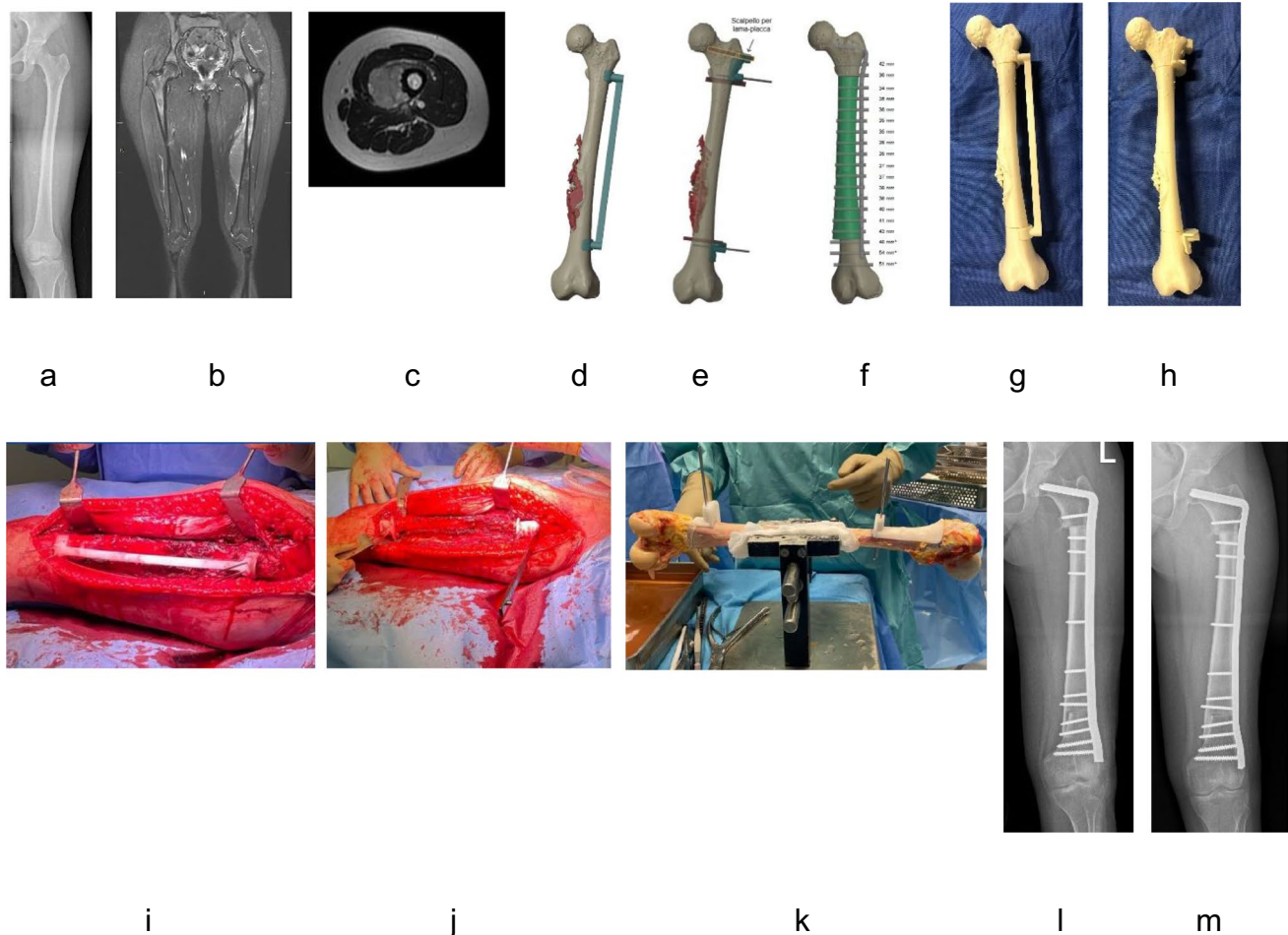


Fig. 1 An example of preoperative planning, design and 3D printing, and intraoperative use of patient-specific cutting guides is shown. The patient was a 17-year-old female with Ewing sarcoma in the left femur. Plain radiographs demonstrated a lytic lesion in the femur (Fig. 1a). Magnetic Resonance Imaging was utilized to evaluate the extraosseous size and intramedullary extension of the tumour (Fig. 1b, c). The models were validated by the surgical team and used for virtual surgical planning in Blender, where resection planes ensuring safe margins (>1 cm) were defined by an engineer in collaboration with the surgeon (Fig. 1d, e). Donor CT scans of MBA were segmented to generate 3D model, which was aligned with the patient's anatomy in Blender to optimise host-graft contact (Fig. 1f).

Anatomical models reproduced the affected bone and the selected donor segment at real scale (Fig. 1g, h) to support surgical planning and verify the proper fitting of the guides. Intraoperatively, adequate bone was exposed to allow secure placement of the patient-specific cutting guide, which was fixed to the native bone with Kirschner wires and osteotomies were then performed (Fig. 1i, j). The graft-specific cutting guide was subsequently applied to the donor bone to harvest the intercalary graft (Fig. 1k), which was then positioned at the resection site and stabilized with internal fixation (Fig. 1l). The time to bone union in the metaphyseal and diaphyseal junction was 3.4 months and 6.2 months, respectively (Fig. 1m)

structures using Materialise Mimics (Materialise, Leuven, Belgium). The models were validated by the surgical team and used for virtual surgical planning into the open-source software Blender (Blender Foundation), where resection planes ensuring safe margins (> 1 cm) were defined by an engineer in collaboration with the surgeon (Fig. 1d, e). The team refined the surgical approach, determined safe cutting levels and optimal osteotomy trajectories, and planned reconstruction strategy using plates. CT scans of multiple candidate donor grafts were segmented following the same workflow used for the patient bone to generate 3D models. The donor models were then aligned to the recipient anatomy in Blender and the graft providing the best anatomical match was selected to optimise host–graft contact (Fig. 1f). The resection cutting planes defined on the patient model were transferred to the donor bone, serving as geometric references for GSI design. Several iterative planning sessions between the surgeon and engineer allowed the simulation of resection scenarios, including evaluation of the surgical approach and incision placement, leading to the selection of the most feasible and accurate solution.

Design and 3D printing

The design and 3D-printing of patient-specific models and instruments were categorized into three groups: anatomical models of the patient and donor, patient-specific cutting guides, and graft-specific cutting guides. Anatomical models reproduced the affected bone and the selected donor segment at real scale (Fig. 1g, h) to support surgical planning and verify the proper fitting of the guides. Cutting guides were developed to improve precise osteotomy and included fixation holes positioned to avoid tumour contact. In cases requiring blade plates, additional slots allowed chisel insertion for plate osteosynthesis. Both patient- and donor-specific cutting guides featured support bases to stabilize the saw blade during osteotomy. Anatomical models were designed in Blender and fabricated using FDM 3D printing technology (Bambu Lab X1C, Bambu Lab, Shenzhen, China) with polylactic acid (PLA) filament (FiloAlfa®). Cutting guides were designed in PTC Creo Parametric (PTC Inc., Boston, MA, USA) based on the digital bone surface and on the predefined osteotomy planes, using standard Computer-Aided Design operations and printed with FDM technology (Qidi i-Mates, Qidi Tech, Zhejiang, China) using PLA Crystal filament (Fillamentum®). The main 3D-printing parameters are summarized in Table 2. Segmentation of a lower limb from CT and MRI datasets required approximately six to eight h in total, considering both patient and donor imaging set. Preoperative planning with the surgeon typically involved three meetings, each lasting one to 1.5 h, during which medical images, digital 3D models, anatomical models, and prototypes of cutting guides were reviewed. The

Table 2 Main 3D-printing parameters

Parameter	FiloAlfa® PLA	Fillamentum® PLA Crystal
Printing Temperature	200 °C	220 °C
Heated Bed Temperature	60 °C	60 °C
Nozzle Diameter	0.4 mm	0.4 mm
Layer Thickness	0.2 mm	0.2 mm
Printing Speed	60 mm/s	60 mm/s
Travel Speed	200 mm/s	150 mm/s
Infill Density	15% Lightning	100% Line
Flow	100%	100%
Cooling	Yes	Yes
Support	Yes	Yes

design of patient-specific cutting guides required approximately 1.5–two h per guide, with each developed sequentially using geometric reference features from the previous one to ensure consistency. For 3D printing, anatomical bone models required on average three to four h per model (6–8 h per case), while definitive cutting guide, printed in sterilizable material, required on average six h. Post-processing included one h of annealing, as recommended in the material datasheet, and an additional one h for support removal and preparation for sterilization. The design and fabrication of patient-specific instruments, including both cutting guides and anatomical models, is a time-consuming process, requiring on average approximately 27.5 to 33.5 non-continuous hours. All cutting guides were sterilized up to two days before surgery and delivered to the operating room on the day of the intervention.

Intraoperative use of patient-specific cutting guides

Adequate bone was exposed to allow secure placement of the PSI, which was fixed to the native bone with Kirschner wires (Fig. 1i, j). Positioning was verified by fluoroscopy and direct inspection. In patients requiring a reconstruction using blade plate, a chisel groove was created through additional guide slots. Osteotomies were then performed using power oscillating saws, and residual soft tissues were carefully dissected to allow en bloc removal of both bone and guide. The GSI was subsequently applied to the donor bone to harvest the intercalary graft (Fig. 1k), which was then positioned at the resection site and stabilized with internal fixation (Fig. 1l, m).

Clinical and radiographic follow-up

Children underwent radiographic follow-up every three months until bone union of MBA was achieved. Bone

union was defined based on modified Radiographic Union Score for Tibia (mRUST) score of 9 on both anteroposterior and lateral radiographs [17]. Bone union was independently assessed by EN and AA who were not involved in the index surgical procedure. In cases of discrepancy between the two assessments, a consensus reading was performed through joint review to reach a final decision. The time of bone union was also assessed.

Assessment of study outcomes

The length of the resected specimen was compared with the length of preoperatively planned bone resection to investigate the accuracy of patient-specific cutting guides [8]. The resected specimen was radiographed, and its length was measured based on the X-ray image. In case where X-rays was not taken, the value recorded in the pathological report was used as the resection length. The type and frequency of surgical complications were documented. The functional results were evaluated according to the Musculoskeletal Tumour Society (MSTS) 93 score [18]. The Mann–Whitney U test was used to analyse continuous parameters. For all analyses, associations were considered significant at a $P < 0.05$, and the Bell Curve for Excel (Social Survey Research Information Co., Ltd., Tokyo, Japan) was used.

Ethical approval

Ethical approval for this study was obtained from the Ethic Committee of Area Vasta Emilia Centro (CE AVEC: 301/2022/Sper/IOR).

Results

3D-printed cutting guides

Cutting guides were used in all patients included in this study. On average, three to four cutting guides were employed per case, accounting for both the patient and the donor graft. No mechanical issues, fractures, deformations, or other alterations affecting guide usability were reported.

Surgical treatment, margins, and accuracy

Intercalary resections were performed using PSIs and the reconstruction was made with an intercalary MBA shaped using GSI in all children. In two children, 3D-printed PSIs were designed with an integrated blade groove to guide also the osteosynthesis with a blade plate. Internal fixation was achieved with a plate in all children. The median surgical time was 232 min (range 195–264 min). The surgical margins were R0 in all children. The median length of

preoperatively planned bone resection and resected specimen was 16.5 cm (range 15.0–23.5 cm) and 16.8 cm (range 16.0–23.5 cm), respectively. The median difference in bone length was 0.2 cm, ranging from 0–0.4 cm ($p = 0.81$) (Table 1). No local recurrence or distant metastases were observed at the latest follow-up.

Bone union

Bone union was achieved in 13 out of 14 (92.9%) osteotomy sites, with only one non-union at the diaphyseal junction. The median time to bone union in the metaphyseal and diaphyseal junction was 5.3 months (range 3.0–6.5 months) and 8.7 months (range 6.2–10.8 months), respectively ($p = 0.01$).

Complications

One of seven children (14.3%) presented delayed union at the diaphyseal junction which was successfully treated with a strut allograft six months after the initial surgery. No other complications were observed.

Functional outcomes

At the latest follow up, the median MSTS Score was 30 (range, 23–30).

Discussion

Previous studies showed that 3D-printed patient-specific cutting guides enabled accurate multiplanar osteotomies in complex areas like the pelvis while reducing operative time and blood loss [1]. In addition, these 3D-printed patient-specific cutting guides facilitated shaping MBA to match tumour defects, potentially enhancing bone union [10]. In the present series, the use of in-house 3D-printed patient-specific cutting guides designed for both tumour resection and graft reconstruction enabled accurate resection with negative margins and facilitated the accuracy of fit between the host bone and MBA following intercalary resection in children with malignant bone tumours of the lower limb.

Limitations

This study has some limitations. First, the sample size was limited due to the novelty approach of the application of 3D printing technology in paediatric orthopaedic oncology. Second, the follow-up period for children in this study was relatively short, precluding full assessment of long-term oncological outcomes and late complications. However, evaluation of surgical margins, correct planned lengths of resection of the tumour and reconstruction with MBA and

the union of the osteotomy site was feasible, as these parameters do not require long follow-up such as for oncological complication. Third, there is a lack of a control group in this study. However, because sarcomas in children are uncommon, it is very difficult to conduct a prospective study comparing the accuracy of 3D-printed cutting guide and free hand technique in children with malignant bone tumours of lower limb who receive joint-preserving surgery by intercalary resection and reconstruction with MBA. Therefore, the present findings can only be interpreted in comparison with previously published studies analysing intercalary reconstruction with MBA in children with bone tumours who underwent free hand intercalary resection. Fourth, length of resected specimen was primarily determined using postoperative radiographs, and pathological reports were consulted when radiographs were unavailable. Radiographic measurements are susceptible to magnification errors, whereas pathological measurements may be influenced by residual soft tissue and formalin-induced shrinkage. This heterogeneity in measurement methods may have introduced bias in the assessment of resection accuracy. Although the discrepancy between the planned and actual resection lengths was small, these methodological differences should be taken into account when interpreting the precision of the cutting guides. Finally, the authors attempted to clarify the context of their findings by comparing the results with historical control groups reported in the literature. However, inter-study comparisons may be influenced by differences in patient selection, surgical techniques, and outcome assessments; therefore, any definitive conclusions regarding superiority should be drawn with appropriate caution.

Clinical challenges

Malignant bone tumours of the lower limb in children requiring intercalary resection and reconstruction with MBA represent a technically demanding surgery [14]. The main challenges include achieving oncologically safe margins while preserving joint function, obtaining precise multiplanar osteotomies in growing bone, and ensuring optimal host-graft congruency to reduce the risks of non-union, fracture, and implant failure [1]. Conventional freehand techniques or intraoperative navigation systems may still result in geometric inaccuracy and prolonged operative time [19, 20]. The present in-house 3D-printing workflow enables meticulous preoperative planning by repetitive surgeon-engineer collaboration, accurate transfer of resection planes to both host bone and allograft, and preoperative verification of guide fitting. This structured approach improves resection precision, enhances graft fit, and may contribute to lower complication rates and improved functional outcomes in this complex paediatric setting [1].

Surgical treatment, margins, and accuracy

Previous monocentric retrospective studies showed that 3D-printed patient-specific cutting guides achieved negative margin of resection of tumours in long bones in most of the patients (90.1–100%) (Table 3) [5–7]. Previous monocentric retrospective studies focusing on the accuracy of bone resection reported that the difference between the length of preoperatively planned bone resection and the resected specimens ranged from 2.3 mm to 8.4 mm in patients with pelvis and extremity bone tumours using 3D-printed patient-specific cutting guides [8, 12, 21]. In a monocentric retrospective study, 29 patients with malignant primary bone tumour of the pelvis and extremity underwent tumour resection using a custom-made 3D-printed patient-specific cutting guide: the accuracy of bone resection was evaluated by comparing the planned length and the length from the osteotomy site to those of the tumour in the actual resected bone specimens, revealing a difference of 1–3 mm [22]. In our study, all resections achieved R0 margins and the median deviation between planned and actual resection length was only 0.2 cm. These findings are consistent with previous studies. The limited discrepancy observed in our cohort suggests that the integration of the in-house 3D-printing workflow contributes to enhanced geometric accuracy.

Bone union

Intercalary reconstruction with MBA results in non-union in 6–43% of patients [23]. There are few studies focusing on allograft reconstruction following resection of bone tumours using 3D-Printed cutting guides reporting that the achievement of bone union in osteotomy sites was 75–92.3%, with a median time to bone union of 4.8 months [11, 22, 24]. A monocentric retrospective study analysing 6 patients with mean age at surgery of 30.8 years (range, 18–60 years) with malignant primary bone tumour of the diaphysis of femur or tibia who underwent reconstruction with MBA shaped by GSIs following resection using a 3D-printed PSI, showed that bone union was achieved in nine of 12 (75%) of osteotomy sites with a median time of 4.8 months (range 2.3–8.3 months) [22]. In our cohort, bone union rate was achieved in 92.9% of osteotomy sites, with metaphyseal junctions healing earlier than diaphyseal junctions. The high union rate observed may be partially explained by improved host-graft congruency achieved through precise geometric transfer of planned resection planes to the actual ones.

Complications

Previous retrospective studies reported complications in patients who underwent intercalary resection of malignant bone tumours of the femur and tibia with reconstruction

Table 3 Summary of clinical studies of 3D-printed patient-specific cutting guides in orthopaedic oncology

Authors	Patient Number	Site	Histology	Usage of 3D Printing Technology	Negative Margin	Local Recurrence	Complication	MSTS (0–30)	Accuracy of Osteotomy
Wang et al. [4]	33	Femur Tibia	CS, GCT, OS	G	90.9%	9.1%	12.1%	Median: 28 Average: 27	NA
Ma et al. [7]	8	Femur	OS	M/G/R	100%	0%	NA	Average: 27	NA
Wong et al. [5]	3	Femur Tibia	EWS, OS	G/I	100%	0%	0%	Median: 29	The mean maximum deviation errors of the nine achieved bone resections: 1.64 ± 0.35 mm
Park et al. [8]	12	Pelvis, Sacrum, Extremity	CS, Meta, OS, STS	G, G/R, or G/I	100%	8.3%	NA	NA	The mean cutting error for the shortest margin: 1.2 (range 0 to 3) mm. The mean cutting error for the greatest margin: 1.4 (range 0 to 3) mm. The maximal cutting error: 3 mm
Müller et al. [10]	12	Pelvis, Extremity	CS, EWS, OS	G/R	91.7%	0%	NA	NA	The error of osteotomy: 0.74 ± 0.96 mm- 3.60 ± 2.46 mm
Dong et al. [6]	17	Pelvis, Femur, Tibia	EWS, Meta, OS, CS, GCT	M/G, M/G/R, M/G/I, M/G/R/I	93.8%	0%	47.1%	Average: 24	Average difference between planned resection length and resection length: 8.35 mm
Gasparro et al. [9]	6	Femur Tibia	CS, EWS, OS	G/R	100%	0%	50%	NA	NA

M model, *G* resection guide, *R* reconstruction guide, *I* implant

CS chondrosarcoma, EWS ewing sarcoma, GCT giant cell tumor, Meta metastatic tumors, OS osteosarcoma, NS not significant, STS soft-tissue sarcomas, NA not available

using intercalary MBA, with complication risk ranging from 25.5% to 45.7%, including fracture (11.8%–28.6%), non-union (8.6%–23.5%), and deep infection (5.8%–17.6%) [25, 26]. No previous studies analysed the complication of intercalary resection and reconstruction with MBA in children with malignant bone tumours of lower limb treated using in-house 3D-printed patient-specific cutting guide, with only one monocentric retrospective study analysing six adult patients with malignant primary bone tumour of the diaphysis of femur or tibia, reporting five complications in six patients including three non-union (50%) and two implant failure (33.3%) [11]. In our series, only one complication (non-union in one out of 14 osteotomy sites) was observed and successfully treated adding bone autografts from iliac bone, with no other complications. Although the small sample size precludes definitive conclusions, these preliminary findings suggest that accurate osteotomies and improved host-graft contact may help reduce risk of inadequate margins or non-union. Moreover, the absence of procedure-related issues implies that in-house cutting guides do not introduce additional risks and that their use is not associated with an increased incidence of infection.

Functional outcomes

Previous studies focusing on joint-sparing tumour resection of malignant bone tumours of the femur and tibia and reconstruction with MBA reported mean MSTS score of 26–27 [25, 26]. A monocentric retrospective study analysing 35 patients who underwent joint-preserving resection of osteosarcoma and MBA reconstruction of the distal femur and proximal tibia showed mean functional score of 26 [25]. Our favourable functional outcome is consistent with previous studies, with the median MSTS score being 30, showing that intercalary reconstruction may be associated with very good functional results in children due to the preservation of adjacent joints.

In conclusion, in-house 3D-printed patient-specific cutting guides for tumour resection and intercalary graft reconstruction with MBA demonstrated high accuracy in achieving negative margins and precise host-graft matching in children undergoing intercalary reconstruction for malignant bone tumours of the lower limb. In this paediatric oncologic setting, an integrated in-house 3D-printing workflow represents a structured and reproducible approach to enhance surgical precision reducing surgical time and possible complications such as non-union.

Author Contribution E.N., G.A., C.E. and T.O. conceived and designed the study. E.N., G.A., G. M., and G.T. analyzed the data. E.N. and E. C. performed statistical analysis. E.N., G.A., and G.M. wrote the main manuscript text. All authors reviewed the manuscript.

Funding Open Access funding provided by Okayama University. This work was supported by JSPS KAKENHI (grant nos. 24K1045306 and 25K2266007).

Data Availability No datasets were generated or analysed during the current study.

Declarations

Ethics approval and consent to participate This prospective study involving human participants was in accordance with the ethical standards of the institutional and national research committee and with the 1964 Helsinki Declaration and its later amendments or comparable ethical standards. Ethical approval was obtained from the Institutional Review Board.

Competing interests The authors declare no competing interests.

Open Access This article is licensed under a Creative Commons Attribution 4.0 International License, which permits use, sharing, adaptation, distribution and reproduction in any medium or format, as long as you give appropriate credit to the original author(s) and the source, provide a link to the Creative Commons licence, and indicate if changes were made. The images or other third party material in this article are included in the article's Creative Commons licence, unless indicated otherwise in a credit line to the material. If material is not included in the article's Creative Commons licence and your intended use is not permitted by statutory regulation or exceeds the permitted use, you will need to obtain permission directly from the copyright holder. To view a copy of this licence, visit <http://creativecommons.org/licenses/by/4.0/>.

References

1. Aiba H, Spazzoli B, Tsukamoto S et al (2023) Current concepts in the resection of bone tumors using a patient-specific three-dimensional printed cutting guide. *Curr Oncol* 30:3859–3870. <https://doi.org/10.3390/curroncol30040292>
2. Lv Z, Li J, Yang Z et al (2023) A novel three-dimensional-printed patient-specific sacral implant for spinopelvic reconstruction in sacral giant cell tumour. *Int Orthop* 47:1619–1628. <https://doi.org/10.1007/s00264-023-05759-0>
3. Jovičić MŠ, Vuletić F, Ribičić T et al (2021) Implementation of the three-dimensional printing technology in treatment of bone tumours: a case series. *Int Orthop* 45:1079–1085. <https://doi.org/10.1007/s00264-020-04787-4>
4. Hu H, Liu W, Zeng Q et al (2019) The personalized shoulder reconstruction assisted by 3D printing technology after resection of the proximal humerus tumours. *Cancer Manag Res* 11:10665–10673. <https://doi.org/10.2147/CMAR.S232051>
5. Liu W, Shao Z, Rai S et al (2020) Three-dimensional-printed intercalary prosthesis for the reconstruction of large bone defect after joint-preserving tumor resection. *J Surg Oncol* 121:570–577. <https://doi.org/10.1002/jso.25826>
6. Wang F, Zhu J, Peng X, Su J (2017) The application of 3D printed surgical guides in resection and reconstruction of malignant bone tumor. *Oncol Lett* 14:4581–4584. <https://doi.org/10.3892/ol.2017.6749>
7. Wong KC, Sze LKY, Kumta SM (2021) Complex joint-preserving bone tumor resection and reconstruction using computer navigation and 3D-printed patient-specific guides: a technical note of three cases. *J Orthop Translat* 29:152–162. <https://doi.org/10.1016/j.jot.2021.05.009>

8. Dong C, Beglinger I, Krieg AH (2022) Personalized 3D-printed guide in malignant bone tumor resection and following reconstruction – 17 cases in pelvic and extremities. *Surg Oncol* 42:101733. <https://doi.org/10.1016/j.suronc.2022.101733>
9. Ma L, Zhou Y, Zhu Y et al (2016) 3D-printed guiding templates for improved osteosarcoma resection. *Sci Rep* 6:23335. <https://doi.org/10.1038/srep23335>
10. Park JW, Kang HG, Lim KM et al (2018) Bone tumor resection guide using three-dimensional printing for limb salvage surgery. *J Surg Oncol* 118:898–905. <https://doi.org/10.1002/jso.25236>
11. Gasparro MA, Gusho CA, Obioha OA et al (2022) 3D-printed cutting guides for resection of long bone sarcoma and intercalary allograft reconstruction. *Orthopedics*. <https://doi.org/10.3928/01477447-20211124-07>
12. Müller DA, Stutz Y, Vlachopoulos L et al (2020) The accuracy of three-dimensional planned bone tumor resection using patient-specific instrument. *CMAR Volume 12*:6533–6540. <https://doi.org/10.2147/CMAR.S228038>
13. Wittekind C, Compton C, Quirke P et al (2009) A uniform residual tumor (R) classification: integration of the R classification and the circumferential margin status. *Cancer* 115:3483–3488. <https://doi.org/10.1002/cncr.24320>
14. Trisolino G, Depaoli A, Menozzi GC et al (2023) Virtual surgical planning and patient-specific instruments for correcting lower limb deformities in pediatric patients: preliminary results from the in-office 3D printing point of care. *J Pers Med* 13:1664. <https://doi.org/10.3390/jpm13121664>
15. Menozzi GC, Depaoli A, Ramella M et al (2024) High-temperature polylactic acid proves reliable and safe for manufacturing 3D-printed patient-specific instruments in pediatric orthopedics—results from over 80 personalized devices employed in 47 surgeries. *Polymers* 16:1216. <https://doi.org/10.3390/polym16091216>
16. Alessandri G, Frizziero L, Santi GM et al (2022) Virtual surgical planning, 3D-printing and customized bone allograft for acute correction of severe genu varum in children. *JPM* 12:2051. <https://doi.org/10.3390/jpm12122051>
17. Coburn A, Shearer D, Albright P et al (2021) Evaluating reliability and validity of the modified radiographic union scale for tibia (mRUST) among North American and Tanzanian surgeons. *OTA Int Open Access J Orthop Trauma* 4:e093. <https://doi.org/10.1097/OI9.0000000000000093>
18. Marchese VG, Rai SN, Carlson CA et al (2007) Assessing functional mobility in survivors of lower-extremity sarcoma: reliability and validity of a new assessment tool. *Pediatr Blood Cancer* 49:183–189. <https://doi.org/10.1002/pbc.20932>
19. Bruschi A, Donati DM, Di Bella C (2023) What to choose in bone tumour resections? Patient specific instrumentation versus surgical navigation: a systematic review. *J Bone Oncol* 42:100503. <https://doi.org/10.1016/j.jbo.2023.100503>
20. Tsukamoto S, Mavrogenis AF, Masunaga T et al (2023) Megaprosthesis reconstruction of the distal femur with a short residual proximal femur following bone tumor resection: a systematic review. *J Orthop Surg Res* 18:68. <https://doi.org/10.1186/s13018-023-03553-7>
21. Scorianz M, Scoccianti G, Guariento L et al (2024) Joint-sparing resection of juxta-articular primary tumors of the knee using titanium alloy 3D-printed cutting guides and allograft reconstruction. *Cancers* 16:4185. <https://doi.org/10.3390/cancers16244185>
22. Lee SH, Kim W, Lee JS (2023) What are the resection accuracy and guide-fitting errors associated with 3D-printed, patient-specific resection guides for bone tumour resections? *Bone Joint J* 105-B:190–197. <https://doi.org/10.1302/0301-620X.105B2.BJJ-2022-0585.R2>
23. Errani C, Tsukamoto S, Almunhaisen N et al (2021) Intercalary reconstruction following resection of diaphyseal bone tumors: a systematic review. *J Clin Orthop Trauma* 19:1–10. <https://doi.org/10.1016/j.jcot.2021.04.033>
24. Butler ZR, Riley DJ, Gusho CA et al (2026) Long-term outcomes of 3-dimensional-printed cutting guides for long bone sarcoma resection and intercalary allograft reconstruction: an updated case series. *Orthopedics*. <https://doi.org/10.3928/01477447-20260106-02>
25. Aponte-Tinao L, Ayerza MA, Muscolo LD, Farfalli GL (2015) Survival, recurrence, and function after epiphyseal preservation and allograft reconstruction in osteosarcoma of the knee. *Clin Orthop Relat Res* 473:1789–1796. <https://doi.org/10.1007/s11999-014-4028-5>
26. Huang M, Ma Z, Yu J et al (2023) Does joint-sparing tumor resection jeopardize oncologic and functional outcomes in non-metastatic high-grade osteosarcoma around the knee? *World J Surg Oncol* 21:185. <https://doi.org/10.1186/s12957-023-03045-2>

Publisher's Note Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.