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Estimation of average and maximum daily-life mobility performance using the Timed Up-and-Go (TUG):  
Exploring the added value of an instrumented TUG

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1 **Estimation of average and maximum daily-life mobility performance**  
2 **using the Timed Up-and-Go (TUG): Exploring the added value of an**  
3 **instrumented TUG**

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19 Short Title: Estimation of daily-life mobility performance in community-dwelling older adults

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32

33 Motor capacity; mobility performance; TUG;

## 34 Abstract

### 35 Introduction:

36 The association between specific motor capacity variables obtained in a laboratory and parameters of  
37 daily-life mobility performance obtained via wearables is still unclear. The Timed Up-and-Go (TUG)  
38 test is a widely used motor capacity tests available either as traditional hand-stopped TUG or as  
39 instrumented TUG (iTUG) providing specific information about its subphases. This study aimed to: 1)  
40 estimate the association between the TUG and specific parameters reflecting average and maximum  
41 daily-life mobility performance (MP), 2) estimate the benefits of the iTUG in terms of explaining MP in  
42 daily life compared to the TUG.

### 43 Methods:

44 The present study was a cross-sectional analysis using baseline data of 294 older persons (mean  
45 age:  $76.7 \pm 5.3$  years). Univariate linear regression analysis was performed to delineate the coefficient  
46 of determination between TUG time and participants' MP. MP variables containing mean cadence  
47 (MCA) to represent average performance and the 95th percentile of mean cadence of walks with more  
48 than three steps ( $p95 > 3\text{stepsMCA}$ ) to represent maximum performance. To determine whether the  
49 iTUG variables give more information about MP, a stepwise multivariate regression analysis between  
50 iTUG variables and the  $p95 > 3\text{stepsMCA}$  variable to represent maximum performance was conducted.

### 51 Results:

52 The univariate regression models revealed associations of the TUG with MCA (adjusted  $R^2 = .078$ ,  
53  $p < 0.001$ ) and  $p95 > 3\text{stepsMCA}$  (adjusted  $R^2 = .199$ ,  $p < 0.001$ ). The multivariate stepwise regression  
54 models revealed a total explanation of maximum daily life MP ( $p95 > 3\text{stepsMCA}$ ) of the TUG (adjusted  
55  $R^2 = .199$ ,  $p < 0.001$ ) vs. iTUG (adjusted  $R^2 = .278$ ,  $p < 0.010$ ).

### 56 Discussion/ Conclusion:

57 This study shows that the TUG better reflects maximum daily life MP than average daily life MP.  
58 Moreover, we demonstrate the added value of the iTUG for a more accurate estimation of daily MP  
59 compared to the traditional TUG. The iTUG is recommended to estimate maximum daily life MP in fall-  
60 prone older adults. The study is a step toward a specific assessment paradigm using capacity  
61 variables from the iTUG to estimate maximum daily life MP.

## 62 Introduction

63 Understanding the association between what people are able to do during a specific motor  
64 assessment in a standardized environment and what people do in their daily life is important in order  
65 to develop specific laboratory-based assessments capturing relevant aspects of daily functioning [1].  
66 The International Classification of Function, Disability, and Health (ICF) [2] discriminates between  
67 assessments measuring motor capacity (MC), which is indicative of the highest possible level of  
68 functioning of an individual in each moment in time, and in contrast, real-life assessments measuring  
69 mobility performance (MP) which is what an individual does in their current environment. Typically, MC  
70 tests are conducted in standardized settings, often using stopwatch timing, or counting repetitions of  
71 movements or tasks [1].

72 In clinical practice, MC measures (e.g., habitual gait speed) are often used to draw conclusions on  
73 subjects' MP and functionality in real life, reflecting their performance beyond the time of the  
74 assessment [3]. This is crucial as clinical decisions leading to subsequent therapeutic interventions or  
75 the initiation of a rehabilitation chain are often based on such laboratory-based test results [3].

76 However, previous studies show that MC measures in older adults such as habitual gait speed have  
77 limited value for predicting MP in real-life [4–8]. In other words, the relationship between MC and MP  
78 is not straightforward. Among several factors influencing the association between MC and MP habitual  
79 vs. maximal performance conditions have been identified as important factors. For example, gait  
80 parameters measured in the laboratory, (e.g., 4m gait speed, cadence) reflect a person's best MP  
81 rather than their average MP [9]. More specifically, older people's habitual gait speed measured in the  
82 laboratory is more closely related to the maximum gait speed than to average gait speed in the real  
83 world. This could be explained by the fact that walking under laboratory conditions can increase the  
84 awareness of being observed, which is known as the Hawthorne effect [10]. Current research has  
85 focused on the MC-MP association with a focus on laboratory-based assessment of gait speed [9, 11,  
86 12].

87 In contrast, the relationship between the Timed-Up-And-Go (TUG) and average and maximum MP  
88 measures, which represent real life performance, is less clear. This is surprising as the TUG is a  
89 widely used laboratory-based capacity test to evaluate mobility performance and proactive balance  
90 control [13]. Compared to habitual gait speed, the TUG includes key motor functions in addition to  
91 habitual gait speed, such as getting up and sitting down from a chair, which are highly important for

92 daily life [18]. The TUG is easy to administer and able to discriminate between fallers and multiple  
93 fallers [14]. Therefore, it is of clinical importance to understand the relationship between TUG and real-  
94 life performance. Longer TUG times have been associated with impaired mobility and an increased fall  
95 risk in older patients and patients with Parkinson's disease or stroke [15–17]. The TUG consists of four  
96 subcomponents (sit-to-stand, gait, turning and turn-to-sit), that have an essential meaning for the  
97 patient's daily life [18]. A drawback is that the traditional TUG solely looks at the total time to complete  
98 the test without separating the subject's performance into the four individual components [19] although  
99 there is additional clinical information to be drawn from data on the subcomponents. However, total  
100 TUG time is not necessarily, and at most only very slightly, associated with the performance of the  
101 specific subcomponents [18].

102 As a result, the TUG only provides limited information about the underlying reasons for reduced total  
103 performance [18, 20]. For example, it has been found that the features that capture the turning phases  
104 are particularly relevant, as they may be important for predicting balance and they have been shown  
105 to be particularly sensitive as they may explain impaired motor control in patients at risk of falling  
106 and/or those with mild cognitive impairment [21, 22]. This is because the turning task with its  
107 asymmetric characteristics of the turning phases requires a certain amount of turning speed, stride  
108 length, stride width and precise control of the individual limbs in order to keep the centre of gravity  
109 between the two feet. For this reason, the turning task particularly endangers the patient's postural  
110 control, e.g. in patients with Parkinson's disease. The new, instrumented version of the TUG (iTUG)  
111 aims to overcome the aforementioned limitations by using inertial sensors to compute a set of spatial  
112 and temporal features from different subphases [23] of the iTUG that can be used to examine the  
113 quality of the task in more detail [21, 22]. The iTUG can compute specific features for the turning  
114 phases, such as the Mean Velocity Turn to Sit, Peak Velocity, or turning duration [21]. Overall, the  
115 iTUG is able to compute a high number of features [24]. Through a factor analysis, Coni et al. were  
116 able to reduce the dataset to 38 instrumented features (Tab. 5) with a clear clinical meaning, which  
117 were grouped into eight factors [24]. The eight factors of the interpretative model according to Coni et  
118 al. are "walking ability", "postural transitions intensity anterior-posterior direction", "sit-to-walk  
119 smoothness", "turn-to-sit smoothness", "turning ability", "global fitness", "turn-to-sit intensity vertical  
120 direction", "sit-to-walk intensity medio-lateral direction". Based on the underlying instrumented features  
121 of these factors that provide additional information, we hypothesise that the iTUG may add more value  
122 to the explanation of daily life mobility performance than the TUG. The aim of the present study was to

123 investigate (1) the association between the TUG and specific parameters reflecting average and  
124 maximum daily-life MP and to (2) estimate the benefits of the iTUG in terms of explaining MP in daily  
125 life compared to the TUG.

126

127 ~~For aim (1) we hypothesised that the TUG would show a greater association with maximum MP~~  
128 ~~compared to average MP. For aim (2), we hypothesised that the iTUG would explain a greater amount~~  
129 ~~of coefficient of determination in MP compared to the traditional TUG.~~

130

## 131 Material and Methods

### 132 Population

133 Baseline data of the LiFE-is-LiFE trial [25] were analyzed. Community-dwelling older adults aged 70  
134 years who were 1) cognitively intact (Montreal Cognitive Assessment [MoCA]  $\geq$  23 points [26]), 2)  
135 able to walk 200 meters (with a walker if needed), and 3) did not exercise more than once per week or  
136 engage in more than 150 minutes per week of moderate to vigorous physical activity in the past 3  
137 months, and 4) at risk of falls were included. Detailed information about the inclusion and exclusion  
138 criteria is provided elsewhere [25]. Prior to participation, all participants provided written informed  
139 consent. Ethical approval was given by both responsible Ethic Review Boards of the two study centers  
140 (Heidelberg and Tübingen, Germany). The study agreed with the Declaration of Helsinki.

### 141 Descriptive Measures

142 Demographic and clinical characteristics including age, sex, height, Body-Mass Index (BMI), number  
143 of comorbidities, number of medications, % of fallers in past six months [27], cognitive status (MoCA),  
144 subjective capacity (Late-Life Function and Disability Instrument [LLFDI]) [28], fear of falling (Falls  
145 Efficacy Scale-International, 7-item version [Short-FES-I]) [29], and balance self-efficacy (Activities-  
146 specific Balance Confidence Scale [ABC-Scale]) [30] were collected.

### 147 TUG and iTUG

148 During the TUG, participants were asked to stand up from a standard chair with armrest (height: 45  
149 cm), walk three meters at a comfortable and safe speed, turn around, walk back to the chair, and sit  
150 down [31]. The time (in seconds) needed to complete the test was recorded using a stopwatch.

151 The iTUG variables were collected with a smartphone on the participants' lower back (at the level of  
152 the 5<sup>th</sup> lumbar spine) thru a waist-worn elastic belt. The smartphone-based system was developed  
153 within the FARSEEING project [32]. A custom Android application [23] running on the smartphone  
154 (Galaxy SIII, Samsung, sampling frequency 100 Hz, accelerometer  $\pm 2g$ , gyroscope  $\pm 250^\circ / s$ ) was  
155 used for recording the signals from the triaxial gyroscope and accelerometer embedded within the  
156 smartphone [21, 23]. The assessor controlled a second smartphone, which was connected via  
157 Bluetooth to the smartphone worn by the participant to start and stop the recording of the iTUG.  
158 Inertial signals were processed in MATLAB 2019b (MathWorks, Natick, MA, USA) to identify the four  
159 subphases of the TUG (Sit-to-Walk, Walk, 180Turn, and Turn-to-Sit) and to extract a set of  
160 instrumented features [23]. The interpretation model according to Coni et al. was used to select the 38  
161 variables from the large number of parameters provided by iTUG [24].

162 Sensor-based monitoring of mobility performance

163 The MP parameters were assessed using the triaxial accelerometer "activPAL4™ micro" (PAL  
164 Technologies Ltd., Glasgow, Scotland) continuously worn on the central front right thigh for nine  
165 consecutive days. The first and last day of the assessment period were excluded and only days with  
166 24 hours measurement were included in the analysis. The instrument is able to derive valid body  
167 posture (sitting/lying, standing/upright) and various walking activities (e.g., cadence, steps per day)  
168 from raw data [33]. There is no consensus on which variables are most appropriate for different  
169 purposes [34]. However, it has been shown that walking duration as a parameter seems to be a  
170 surrogate to measure physical activity [35] and it is a well-understood term for communicating with  
171 patients [36]. When measuring walking duration, intensity seems to be an important factor, as walking  
172 can be performed at different levels from light to brisk [37]. To indicate walking intensity, cadence, as a  
173 rate to represent quantified steps displayed over time [38], is an established temporal gait parameter  
174 which is strongly ( $r=0.94$ ) and consistently associated with physical activity intensity [39–42].  
175 Therefore, cadence was chosen as the variable for MP in the present study. From the raw data, we  
176 calculated the mean cadence (MCA) to represent average MP and the 95th percentile of mean  
177 cadence of walks with more than three steps ( $p_{95}>3stepsMCA$ ) to represent maximum MP.

## 178 Statistical Analysis

179 Normal distribution was tested using the Shapiro-Wilk test. ~~Since the instrumented data were not~~  
180 ~~normally distributed, they were log-transformed using the formal natural logarithm in SPSS.~~ Univariate  
181 regressions with MCA and p95>3steps MCA as dependent variables and TUG time as independent  
182 variable were calculated to examine the coefficient of determination between TUG time and  
183 participants' MP. Since the instrumented data were not normally distributed, they were log-transformed  
184 using the formal natural logarithm in SPSS. A stepwise multivariate regression model was used to  
185 determine the benefit of the iTUG in terms of reflection of mobility performance. The p95>3stepsMCA  
186 was used as the dependent variable, and the instrumented variables according to Coni (2018) (Tab. 5)  
187 were used as independent variables. Age, gender, weight, and height were set as control variables for  
188 all regression models. All statistical analyses were performed in SPSS (IBM SPSS Statistics, Version  
189 28. An alpha ( $\alpha$ ) level of 0.05 was used for all statistical tests.

190

## 191 Results

### 192 Descriptive Results

193 A total of 294 participants (sample 1) conducted the TUG and completed the MP measurement. The  
194 participants' mean (SD) age was 78.8 (5.4) and the majority of participants was female (72.8%). The  
195 sample on average was cognitively intact (MoCA score [SD] = 26.0 [2.0] points), had a low fear of  
196 falling (Short FES-I score [SD] = 10.4 [3.0] points), with 41.2% having a fall event in the past 6 months.  
197 The time to complete the TUG (SD) averaged 12.3 (3.4) seconds and the mean cadence (SD) of the  
198 participants in everyday life was 65.1 (6.0) steps per minute.

199 For the multiple regression, only the data from 278 participants (sample 2) could be used, because of  
200 incomplete iTUG measurement. The samples did not differ significantly from each other in any  
201 participant characteristic (data not shown). Table 1 and table 2 present further participant  
202 characteristics and MC and MP parameters of sample 1 and sample 2.

### 203 Association between TUG and average vs maximum mobility performance

204 Table 3 shows the associations between TUG duration and parameters related to average MP (MCA)  
205 and maximum MP (p95MCA, p95>3stepsMCA). For MCA a coefficient of determination of  $R^2 = .078$   
206 was found. However, TUG duration can explain  $R^2 = .199$  of the coefficient of determination for  
207 p95>3stepsMCA.

### 208 Association between iTUG and maximum mobility performance

209 Multiple stepwise regression showed that iTUG data were more strongly associated with maximum  
210 cadence than stopwatch-based TUG time. The strongest model (Tab. 4) showed a coefficient of  
211 determination with an adjusted  $R^2 = .278$  ( $p = .010$ ) compared to  $R^2 = .199$  (TUG, Tab. 3). In addition  
212 to the control variables, the model consists of the following variables: *total duration*, *number of steps*,  
213 *root mean square of vertical acceleration during the turn-to-sit*, *mean angular velocity of the 180° turn*  
214 *and walking duration*. These variables are part of the factors: "walking ability", "turn-to-sit intensity  
215 vertical direction" and "turning ability", where the factor "walking ability" is reflected with all its  
216 variables. The highest beta coefficients were found for the *total number of steps* ( $b = .646$ ) and the  
217 *mean angular velocity of the 180° turn* ( $b = .385$ ).

## 218 Discussion/Conclusion

219 This study aimed to better understand the association between MC measured by the TUG and MP  
220 quantified by sensor-based physical activity monitoring. Results of our first analysis suggest that the  
221 TUG better represents *maximum* MP as compared to *average* MP. Results of our second analysis  
222 suggest an added value of the iTUG for a more accurate estimation of MP compared to the original  
223 TUG.

224 Association between TUG and average vs maximum mobility performance

225 Based on previous research in the field of gait assessment, we hypothesised that the TUG would  
226 show a greater association with maximum MP compared to average MP. This hypothesis was  
227 confirmed by our analysis showing a greater coefficient of determination ( $R^2 = .199$ ) between TUG  
228 time and sensor-derived parameters reflecting everyday life maximum MP (i.e.,  $p95 > 3\text{stepsMCA}$ ) as  
229 compared to parameters reflecting average MP (MCA,  $R^2 = .078$ ). Our results indicate that the TUG  
230 provides specific information about a person's ability to carry out maximum performance tasks in the  
231 real world. The parameter  $p95 > 3\text{stepsMCA}$  reflects those walking episodes with the fastest cadence  
232 carried out in everyday life during the one-week sensor-based assessment period. The fact that this  
233 parameter explained a higher proportion of the variation of the TUG time suggests that mobility  
234 performance measured in the lab is more strongly associated with a person's ability to carry out daily  
235 motor tasks with maximum performance.

236 Our findings are in line with other recently published studies indicating that the MC-MP relationship  
237 differs for average vs. maximum performance. Gordt et al. 2020 found greater correlations ( $r = 0.31$ )  
238 between MC (gait speed) and MP at higher intensities ( $\geq 3\text{MET}$ ) as compared to low intensity  
239 activities ( $\leq 3\text{MET}$ ) ( $r = 0.15$ ) measured over the course of one week [4]. Like in our study, this  
240 demonstrates that MC better reflects a variable representing maximum MP as compared to average  
241 MP.

242 Recently, Wright et al. (2022) found that movement intensity is the most significant parameter of the  
243 MC-MP relationship [8], suggesting that studies on the MC-MP relationship can be enhanced with the  
244 addition of an intensity measure. Our study demonstrates the validity of this statement and supports  
245 the importance of selecting MP variables representing maximum performance in everyday life.

246 Association between iTUG and average vs maximum mobility performance

247 We hypothesised that the iTUG would explain a greater coefficient of determination in MP compared  
248 to the traditional TUG. This hypothesis was confirmed by our analysis showing a greater coefficient of  
249 determination ( $R^2=.278$ ) between everyday MP (p95>3stepsMCA) and specific iTUG variables as  
250 compared to TUG time ( $R^2 = .199$ ).

251 We found that three out of the eight additional iTUG factors provided additional information as  
252 compared to TUG time only. The iTUG factor “walking ability” represented by the features *total*  
253 *duration*, *total number of steps* and *walking duration* was most strongly represented in the model. The  
254 strong representation of walking can be explained with the fact that our MP measure was also  
255 walking-related (cadence in daily life). We found that those who walked faster during iTUG  
256 assessment had a higher MP in daily life. This is in line with Callisaya et al. 2018, who suggest that  
257 slower lab-based normal walking speed compared to complex mobility tasks in older people is the  
258 strongest predictor of shorter daily distances walked, smaller life space, greater impairment in ADLs,  
259 fear of falling, and lower balance confidence [6].

260 In addition to the “walking ability” factor, we identified two iTUG factors related to turning performance  
261 explaining an additional amount of MP variance and increasing the coefficient of determination (i.e.,  
262 “turn-to-sit intensity vertical direction” and “turning ability”). The highest beta coefficient was found for  
263 *mean angular velocity of the 180° turn* feature ( $b = .385$ ). Our findings suggest that the intensity of the  
264 movement increases/decreases with a more confident/cautious approach and that this is reflected in  
265 the daily MP. This is perhaps no coincidence, as the importance of the turn velocity for predictive or  
266 discriminatory ability has already been recognised in several other studies. Coni et al. 2019 showed  
267 that the iTUG features *walk duration* and *turn-to-sit turning maximum velocity* had significant  
268 discriminative ability on physical function measured by the Late-Life Function and Disability Instrument  
269 in high functioning young seniors [21]. Bergquist et al. 2020 showed that the iTUG was able to predict  
270 the Community Balance and Mobility Scale total score with accuracy of 85.2% (84.9-85.5%) in  
271 community-dwelling healthy seniors and geriatric patients [22]. Six of the ten features with highest  $R^2$   
272 scores were features obtained from the two turning phases of the iTUG (e.g., *mean velocity first turn*,  
273 *mean velocity turn to sit*, *peak velocity turn to sit*). The highest  $R^2$  score was found for *mean velocity*  
274 *first turn* and *walk duration* [22]. Caronni et al. 2018 showed that iTUG turning features are the best  
275 predictors of balance in neurological patients as measured by the Mini-BEST test [18]. The authors  
276 propose *the mean angular velocity during turning* and *the duration of the turn phase* as valid ratio

277 measures of balance [18]. More specifically, we found that a lower turning velocity of the iTUG is  
278 associated with a lower daily life MP. Moreover, we found that if turn duration decreases, daily life  
279 performance increases.

#### 280 Strength and limitations

281 Major strengths of this study are the large sample size, one-week instrumented MP assessment and  
282 the systematic approach for classifying iTUG performance based on an established factor concept  
283 [24]. Limitations are that our variables of MP measures were restricted to walking performance.  
284 Although walking is the most common MP in older adults, we acknowledge that participants may have  
285 been engaged in other MP activities (e.g., swimming, cycling) that the sensor-based assessment did  
286 not account for. Our sensor-based MP assessment does not reveal information about indoor or  
287 outdoor mobility performance. This could be extended in future studies using GPS signals Due to the  
288 cross-sectional design of the study, causal inferences cannot be evaluated, and further longitudinal  
289 studies are needed to show that changes in challenging MP measures are associated with changes in  
290 MC.

#### 291 Conclusion

292 Our study highlights that the MC-MP association depends on the specific outcome variables selected  
293 for representing MC and MP. Our results show a closer relationship between MC measures and MP  
294 measures when using MP measures representing the individuals' maximum performance. In other  
295 words, the MC-MP association becomes more evident if those episodes of daily life MP are selected  
296 for analysis that are closer to the performance limit. Such a "testing the limits" paradigm has been  
297 described previously in several studies in related research fields [43].

298 In relation to our second hypothesis, we conclude that the variables collected by the iTUG provide  
299 additional information useful for estimating an individual's daily MP. This highlights the need for  
300 instrumented MC assessments in older adults and is an important step towards tailored assessments  
301 for this target population. Assessment results could form the basis of specific interventions aimed at  
302 restoring or improving relevant MC, such as walking and turning ability, which in turn could enable  
303 older adults to maintain healthy MP patterns and an active lifestyle.

#### 304 Statements of Ethics

305 This study protocol was reviewed and approved by Ethic Review Board of the

306 Faculty of Behavioral and Cultural Studies at Heidelberg University (document number Schwe2017  
307 2/1–1) and from the Ethic Review Board of the University Hospital and Faculty of Medicine in  
308 Tübingen (document number 723/2017BO2). The study is conforming to the respective policy and  
309 mandates of the Declaration of Helsinki. Participants' written informed consent is obtained from  
310 assessors at their first screening visit at the study site.

311

### 312 Conflict of Interest Statement

313 The authors have no conflicts of interest to declare.

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### 317 Author Contributions

318 Conceptualization: FK-G, PH and MS; Methodology: FK-G, PH and MS; Data analysis and  
319 interpretation: FK-G, AE, PH and MS; Resources: SM; Writing–original draft preparation: PH, AE and  
320 MS; Writing–review and editing: CPJ, FK-G, SM, AE, PH and MS. All authors reviewed and critically  
321 revised the manuscript for important intellectual content and approved the final manuscript.

### 322 Data Availability Statement

323 All data analysed during this study are included in this article. Further enquiries can be directed to the  
324 corresponding author.

325

326

327 

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